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2	on the diagnostic accuracy of stress perfusion cardiovascular magnetic
3	resonance
4	
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### 132 Abstract

133 **Background:** Clinical evaluation of stress perfusion cardiovascular magnetic 134 resonance (CMR) is currently based on visual assessment and has shown 135 high diagnostic accuracy in previous clinical trials, when performed by 136 expert readers or core laboratories. However, these results may not be 137 generalizable to clinical practice, particularly when less experienced readers 138 are concerned. Other factors, such as the level of training, the extent of 139 ischaemia, and image quality could affect the diagnostic accuracy. Moreover, 140 the role of rest images has not been clarified.

141 The aim of this study was to assess the diagnostic accuracy of visual 142 assessment for operators with different levels of training and the additional 143 value of rest perfusion imaging, and to compare visual assessment and 144 automated quantitative analysis in the assessment of coronary artery 145 disease (CAD).

Methods: We evaluated 53 patients with known or suspected CAD referred for stress-perfusion CMR. Nine operators (equally divided in 3 levels of competency) blindly reviewed each case twice with a 2-week interval, in a randomised order, with and without rest images. Semi-automated Fermi deconvolution was used for quantitative analysis and estimation of myocardial perfusion reserve as the ratio of stress to rest perfusion estimates.

153 **Results:** Level-3 operators correctly identified significant CAD in 83.6% of 154 the cases. This percentage dropped to 65.7% for Level-2 operators and to 155 55.7% for Level-1 operators (p<0.001). Quantitative analysis correctly 156 identified CAD in 86.3% of the cases and was non-inferior to expert readers

(p=0.56). When rest images were available, a significantly higher level of
confidence was reported (p=0.022), but no significant differences in
diagnostic accuracy were measured (p=0.34).

160 **Conclusions:** Our study demonstrates that the level of training is the main 161 determinant of the diagnostic accuracy in the identification of CAD. Level-3 162 operators performed at levels comparable with the results from clinical 163 trials. Rest images did not significantly improve diagnostic accuracy, but 164 contributed to higher confidence in the results. Automated quantitative 165 analysis performed similarly to level-3 operators. This is of increasing 166 relevance as recent technical advances in image reconstruction and analysis 167 techniques are likely to permit the clinical translation of robust and fully 168 automated quantitative analysis into routine clinical practice.

169

# 170 Keywords

- 171 Cardiovascular Magnetic Resonance, Stress Perfusion Imaging, Coronary
- 172 Artery Disease, Quantitative assessment, Myocardial Ischemia, Diagnostic
- 173 Accuracy, Training.
- 174

# 175 Abbreviation list

- 176 AHA: American Heart Association
- 177 CAD: coronary artery disease
- 178 CME: Continuous medical education
- 179 CMR: Cardiovascular magnetic resonance
- 180 EACVI: European Association of Cardiovascular Imaging
- 181 ESC: European Society of Cardiology

- 182 LAD: left anterior descending coronary artery
- 183 LCX: left circumflex coronary artery
- 184 LGE: late gadolinium enhancement
- 185 MBF: myocardial blood flow
- 186 MPR: myocardial perfusion reserve
- 187 RCA: right coronary artery
- 188 SCMR: Society for Cardiovascular Magnetic Resonance

#### 189 Background

Stress perfusion cardiovascular magnetic resonance (CMR) is increasingly
used for the evaluation of patients with known or suspected coronary artery
disease (CAD) and has a class I indication for patients at intermediate risk of
CAD according to recent guidelines[1,2].

194 Stress perfusion CMR has been shown to be highly accurate for the detection 195 of CAD, with sensitivity ranging from 75% to 91% and specificity ranging 196 from 59% to 87%[3-5]. It should be noted that in most of these studies, 197 visual assessment has been carried out either by a core laboratory or by 198 expert readers, and therefore the findings may not be generalizable to 199 routine clinical practice. As stress perfusion CMR gains acceptance and 200 becomes more available, it will inevitably be performed in lower volume and 201 less experienced centers.

202 Stress perfusion CMR is typically evaluated by visual assessment. This can be 203 influenced by the extent of ischemia and the presence of areas of relatively 204 preserved perfusion, which can be used as reference[6]. Moreover, image 205 artefacts can complicate the interpretation of the images. Dark rim artefacts, 206 which are commonly observed during stress perfusion, can be misdiagnosed 207 as subendocardial perfusion abnormalities[7], in particular when relatively 208 long acquisition times are used and spatial resolution is low. Moreover, 209 areas of infarction are frequently associated with delayed perfusion[8,9]. 210 The simultaneous evaluation of stress and rest perfusion CMR and late 211 gadolinium enhancement (LGE) images is recommended to identify areas of 212 myocardial infarction improve specificity of the and the 213 interpretation[10,11], and to exclude imaging artefacts[10].

Additionally, it has been suggested that rest perfusion images could play an important role in improving the identification of imaging artefacts when signal abnormalities are present on both stress and rest images[10]. The acquisition of rest images enables quantification of perfusion reserve, but prolongs scan times and requires additional contrast dosing.

Stress perfusion CMR is complex to read and requires significant training and experience, however, the impact of training and experience has not been formally studied and as yet, there are no specific recommendations in current guidelines, apart from stating that stress perfusion CMR should be part of the training program for Level-2 readers[12]. It is hoped that fully quantitative automated methods may help bridge training gaps and support clinical decision making.

We sought to determine the importance of the level of operator training of the diagnostic accuracy of stress perfusion CMR; the role of rest perfusion images in the identification of imaging artefacts and in the correct detection of CAD; and to systematically compare the results of visual assessment with semi-automated quantitative analysis to determine its additional value.

231

# 232 <u>Methods</u>

233 Consecutive patients (n=53) referred for stress perfusion CMR for suspected 234 CAD were retrospectively included in the study. All patients had invasive 235 coronary angiography on the basis of the clinical indication within 1 month 236 of the CMR examination. Exclusion criteria were contraindications to CMR, 237 gadolinium-based contrast agents or adenosine. Patients with previous 238 coronary artery bypass grafting, hypertrophic cardiomyopathy, aortic

stenosis, or other primary myopathic or valvular disease were excluded. All
subjects gave written informed consent in accordance with ethical approval.
This study complies with the Declaration of Helsinki.

242

# 243 Image acquisition

244 CMR images were acquired using a 3T scanner (Achieva, Philips Medical 245 Systems, Beth, The Netherlands) equipped with 32-channel phased-array 246 cardiac coil. The protocol included functional assessment, adenosine stress 247 and rest first pass perfusion imaging, and LGE. The images were acquired using standard acquisition protocols and in end-expiratory breath-hold. For 248 249 stress imaging, 140 µg/kg/min of adenosine was administered. Imaging 250 commenced 3 min after infusion initiation. A dual bolus (equal volumes of 251 0.0075 mmol/kg followed by 0.075 mmol/kg after a 20-s pause) of contrast 252 agent (gadobutrol/Gadovist, Schering, Germany) was injected at 4 ml/s by a 253 power injector[13]. For perfusion, a saturation recovery prepared gradient echo pulse sequence accelerated with k-t sensitivity encoding acceleration 254 255 with 11 training profiles was used. Typical imaging parameters were: 3 256 short-axis slices covering standard American Heart Association (AHA) 257 segments[14], 120 acquired dynamics/slice, flip angle 20°, TR 2.5 ms, TE 258 1.25 ms, saturation pre-pulse recovery time 100 ms, pixel size 1.9x1.9 mm, 259 slice thickness 10 mm.

Typical imaging parameters for LGE imaging were: long and short axis to
fully cover the left ventricle, inversion recovery turbo field echo, flip angle
25°, TR 6 ms, TE 3 ms, pixel size 0.7x0.7 mm, slice thickness 10 mm.

263

#### 264 **Operator selection**

265 Nine operators were chosen amongst the physicians working in our unit and 266 in other European institutions, on the basis of their level of competency, 267 according to the European Society of Cardiology (ESC)/European 268 Association of Cardiovascular Imaging (EACVI) training guidelines[12]. A 269 total of 9 operators, 3 for each competency level, were chosen; all operators 270 had recently obtained the ESC/EACVI certification (within 2 months) for the 271 appropriate level. In brief, level-1 competency ESC certification requires 20 272 continuous medical education (CME) hours, involvement in 50 CMR cases 273 and 1-month fellowship; level-2 requires at least 50 CME hours, involvement 274 in 150 clinical cases of which 25 must be perfusion studies, a minimum of 3-275 months fellowship and the European CMR exam; level-3 requires at least 50 276 CME hours, involvement in 300 clinical cases of which a minimum of 50 277 must be perfusion studies, at least 12-months training and the European 278 CMR exam. Level-1 competency reflects core CMR training, level-2 is required to report CMR studies with support from a Level-3 operator and 279 280 Level-3 is required to perform, interpret and report CMR studies fully 281 independently[12].

282

#### 283 Image analysis – visual assessment

Each operator was asked to report each of the 53 scans twice over a 4-week period, with a minimum interval of 2 weeks between first and second read. The scans were anonymized and presented to the operator as a full dataset, including stress and rest perfusion and LGE, or as reduced datasets, including stress perfusion and LGE only. The full and reduced datasets were

analysed blinded to clinical and angiographic data and in a randomizedorder on different days. The study flowchart can be seen in Figure 1.

Visual assessment of adenosine stress perfusion CMR and LGE images, displayed side-by-side, was performed as per clinical practice, in accordance with standardized CMR protocols[15]. A perfusion defect was defined as a regional reduction in myocardial signal during LV first-pass of contrast agent, not related to artefacts and not corresponding to an area of scar on LGE images.

297 Operators were asked to fill an on-line standardized form and to identify 298 segments with inducible ischaemia, to identify the presence and 299 transmurality of LGE[16], to identify the most likely culprit coronary artery 300 based on the standard AHA segmentation[14], and to grade their confidence 301 in the diagnosis and the perceived image quality.

The confidence was graded as: 0- very unconfident, 1- unconfident, 2confident, 3- very confident. The perceived image quality was graded as: 0poor, 1- moderate, 2- good, 3- excellent.

305 Coronary angiography results have been used as reference standard. The 306 threshold for coronary artery lumen stenosis was 70% diameter stenosis for 307 epicardial vessels. All invasive angiographic images have been reviewed by 308 consensus of expert operators.

309

# 310 Image analysis – quantitative assessment

A different operator, blinded to results of visual perfusion assessment and
other clinical/angiographic data, performed the segmentation of the images
for semi-automated quantitative analysis using software and methods

314 previously developed and validated by our group. Respiratory motion was 315 corrected using affine image registration by maximization of the joint 316 correlation between consecutive dynamics within an automatically 317 determined region of interest[17]. A temporal maximum intensity projection 318 was calculated to serve as a feature image for automatic contour delineation 319 method. The operator then manually optimized the automatically generated 320 contours to avoid partial volume effects at the endocardial and epicardial 321 border[17]. The intervention of the operator was limited to image 322 segmentation. Quantitative perfusion analysis was then automatically 323 performed by Fermi-constrained deconvolution according to the methods 324 described by Wilke et al[18] and Jerosch-Herold et al[19], optimised for 325 high-resolution pixel-wise analysis [20,21]. Myocardial perfusion reserve 326 (MPR) was calculated as the ratio between stress and rest myocardial blood 327 flow (MBF) estimates. Ischaemia was defined as segments with MPR<1.5, 328 according to previously validated criteria[22,23].

329

#### 330 Statistical analysis

331 Continuous variables are presented as mean±standard deviation for 332 normally distributed variables and as median with interquartile range for 333 non-parametric data. Normality was assessed with Q-Q plots and the 334 Kolmogorov-Smirnov test. Continuous variables were compared using an 335 unpaired Student *t test* or the Wilcoxon rank-sum test, as appropriate, and 336 categorical data were compared between groups using the Fisher exact test 337 and Pearson chi-square test. The McNemar test was used for paired dichotomous data. Two-tailed values of p<0.05 were considered to be 338

statistically significant. One-way ANOVA was used to determine differences
between multiple groups. Bonferroni correction was used to account for
multiple testing.

342

# 343 <u>Results</u>

## 344 **Characteristics of the population**

345 The mean age of the population (n=53) was  $60.6\pm12.7$  years. Demographic 346 data are shown in Table 1. The prevalence of CAD in the group of patients 347 included in the analysis was 30.2%, with 16/53 patients positive for CAD on 348 invasive coronary angiography. Left anterior descending (LAD) lesions were 349 identified in 9 (17%) of the cases; left circumflex (LCX) lesions in 8 (15.1%) 350 of the cases; and right coronary artery (RCA) in 13 (24.5%) of the cases. 351 Within the group of patients with CAD, 8 patients had 1-vessel disease 352 (50%), 5 patients 2-vessel disease (31.3%) and 3 patients 3-vessel disease 353 (18.8%).

354

#### 355 Impact of operator training on correct CAD identification

356 There was a significant correlation between an operator's training level and 357 the rate of correct identification of CAD on a per patient level on visual 358 assessment. The diagnosis of Level-3 operators agreed with invasive 359 coronary angiography in 83.6±2.3% of the cases, while this percentage 360 dropped to 65.7±4.3% for Level-2 operators and to 55.7±5.3% for Level-1 361 operators (p<0.001 between the 3 groups) (Figure 2). A significant difference 362 in the agreement with angiography between different levels of training was 363 also observed in a sub-analysis per coronary territory (p<0.001)(Figure 3).

When different perfusion territories were compared, the agreement between CMR and coronary angiography was higher for the LAD territory, followed by the LCX and by the RCA territories. The same trend was observed in all groups of operators, regardless of the level of training (p<0.001).

The sensitivity and specificity for operators of different levels of training are reported in Figure 4. Level-1 operators showed high sensitivity ( $86.5\pm6.1\%$ ) and low specificity ( $41.9\pm10.9\%$ ). Level-2 operators had a sensitivity of 57.3±4.7% and a specificity of  $69.4\pm9.9\%$ . Level-3 operators showed a sensitivity of 71.9±13% and a specificity of  $88.7\pm6.7\%$  respectively. There was a statistically significant difference for both sensitivity and specificity between different levels of training (p<0.001)(Figure 4).

376

### 377 Impact of rest perfusion on correct identification of CAD

When rest images were available, there was no statistically significant difference at all levels of training (Figure 5) and in the overall analysis ( $69.6\pm14.3\%$  vs  $67.1\pm13.1\%$ ; p=0.34). However, when rest images were available, a significantly higher level of confidence was reported by the operators (*p*=0.022) and subjective image quality was scored at a higher level (*p*=0.012).

384

### 385 CAD classification

Figure 6 shows a comparison between the extent of CAD identified by the operators on CMR images in comparison with invasive coronary angiography. An overestimation of the severity of CAD was observed in

Level-1 operators, regardless of the number of vessels with CAD. Despite
being more accurate, Level-2 and Level-3 operators significantly
underestimated the number of positive perfusion territories in patients with
multi-vessel CAD.

393

# 394 Impact of quantitative analysis on correct CAD identification

395 Quantitative analysis was successfully performed in 51 patients. In 2 cases of 396 patients without CAD, the automated algorithms failed and no results could 397 be calculated. In both cases, this was due to the low quality of the diluted 398 pre-bolus used for the estimation of the arterial input function. Level-3 399 visual assessment of the 2 cases where quantification failed yielded the 400 correct diagnosis in both cases when both stress and rest images were made 401 available to the readers, and in 66% of interpretations when only stress 402 perfusion was made available to the readers. Quantitative stress perfusion 403 CMR analysis agreed with the results of invasive angiography in 86.3% of the 404 cases, performing significantly better than Level-1 and Level-2 operators 405 (p<0.001). Level-3 visual assessment and quantitative analysis were not 406 significantly different (p=0.56)(Figure 2). Quantitative analysis had a 407 sensitivity of 68.8% and specificity of 94.3%. When the 2 cases in which 408 quantitative analysis failed are considered as a missed diagnosis, the 409 concordance of quantitative analysis with invasive angiography was 83%, 410 with a sensitivity of 68.8% and a specificity of 89.2%.

411

### 412 Discussion

413 This study has several important findings. Operator training and experience 414 had a significant impact on diagnostic accuracy. Only Level-3 trained 415 operators had an accuracy comparable with the results reported by large 416 clinical trials[3-5]. Rest images did not significantly improve the diagnostic 417 accuracy of stress perfusion CMR but, when available, contributed to a 418 significantly higher confidence of the operators in their reports and to a 419 higher perceived image quality, regardless of the level of training. Finally, 420 semi-automated quantitative analysis performed better than Level-1 and 421 Level-2 operators, but similarly to a Level-3 operator. Quantitative analysis however failed in 2/53 cases due to technical reasons related to the 422 423 administration of a diluted pre-bolus. However, the same cases could be 424 analysed visually.

425 Stress perfusion CMR plays an increasingly important role in the evaluation 426 of patients with known or suspected CAD. Recent European guidelines 427 recommend the use of stress perfusion CMR in patients with suspected CAD 428 and intermediate pre-test probability, with a class 1 indication and level of 429 evidence A, similarly to stress echocardiography and nuclear imaging[1,2]. 430 US guidelines recommend stress perfusion CMR with 2A indication[24], 431 particularly in specific subgroups of patients[25]. These indications are 432 based on the assumption that stress perfusion CMR is highly accurate for the 433 identification of CAD and compares favorably with other functional 434 modalities. In large trials and meta-analyses, the sensitivity ranged from 435 75%[3] to 91%[4] and specificity ranged from 59%[3] to 87%[5]. In the CE-MARC study[26], sensitivity was 86.5% and specificity was 83.4%, and the 436 437 MR-IMPACT 2 trial[27] reported a sensitivity of 75% and a specificity of

438 59%. These wide intervals most likely represent the variability in study
439 design, the different prevalence of disease in different populations, and
440 variability in the criteria used for visual assessment.

The diagnostic accuracy of stress perfusion CMR reported in the literature is
often the result of visual assessment carried out by expert readers, which are
usually Level-3 operators and often are internationally recognized experts.
Our study demonstrates that the diagnostic accuracy varied significantly

amongst groups of readers with different levels of training, and reached
values comparable with those of large studies only in the group of Level-3
operators. These results confirm the high diagnostic accuracy of stress
perfusion CMR in comparison with coronary angiography, however clearly
indicate the need for Level-3 supervision when stress perfusion scans are
reported.

451 From the analysis of the sensitivity and specificity for the detection of CAD in 452 different groups, it emerges that Level-1 operators had high sensitivity 453 (86.5%). This came however at the cost of a reduced specificity (41.9%) and 454 rate of overall correct CAD detection (55.7%). Factors such as image quality 455 and the prevalence of dark rim artefacts, which can mimic the presence of 456 subendocardial perfusion defects, could have played a role. In comparison, 457 Level-3 operators under-called the disease (sensitivity 71.9%) but had a 458 high specificity (88.7%). All diagnostic investigations involve a trade-off 459 between sensitivity and specificity. At a population level and from a health-460 economic perspective, we feel that the results achieved by Level 3 operators 461 represent a reasonable balance between the need to identify significant 462 coronary disease and the high specificity required to avoid increasing down-

stream investigation costs through increased referral for invasive coronary
angiography. The work of Patel et al[28] highlights the need for better
selection of patients for invasive investigation given the costs and potential
morbidity incurred by this.

467 Our results support the recommendations from the ESC [12], which state 468 that Level-1 operators hold the basic knowledge in CMR sufficient to select 469 appropriate CMR indications and interpret CMR reports, but are not cleared 470 to report CMR scans. This is reflected in our result by the fact that Level-1 471 operators demonstrated a very low diagnostic accuracy, with poor specificity for the presence of CAD. According to the ESC guidelines, Level-2 472 473 operators may actively perform and report CMR, but are not completely 474 independent and should work under the supervision of a Level-3 expert. 475 This is also supported by our results, since Level-2 operators were 476 significantly less accurate than Level-3 operators. Level-3 operators instead 477 performed to levels similar to those reported by studies such as the CE-MARC[26]. 478

It should be noted that the Society for Cardiovascular Magnetic Resonance (SCMR) guidelines on training[29] differ slightly from the ESC guidelines used in this study to define the level of training of the operators. According to the SCMR guidelines, Level-2 operators can independently report CMR scans, whereas Level-3 certification has more to do with being able to lead a CMR unit and perform research in the field. Both guidelines agree that Level-1 training is not sufficient to practice CMR.

486

It has been suggested that rest perfusion images play an important role in improving the identification of imaging artefacts when signal abnormalities are present on both stress and rest images[10]. When assessing stress perfusion CMR visually, guidelines advise displaying both rest and stress images side-by-side to identify correctly inducible perfusion defect and artefacts[10,11].

In our study, we did not find any significant difference in the diagnostic accuracy when rest images were available. Our findings mirror those of Biglands et al[30]. However, when testing the operator confidence and the perceived image quality, a statistically significant difference was noted when both stress and rest images were available. The increased confidence was more evident for Level-1 and Level-2 operators.

Interestingly, Level-1 operators reported a higher confidence score than
more experienced operators, despite lower overall accuracy. This could
reflect a cognitive bias, also known as the Dunning-Kruger effect[31].

The diagnostic usefulness of rest perfusion imaging resides in the finding of "fixed perfusion defect" on both stress and rest images, which may be related to artefacts or to areas of myocardial infarction. However, this may be overcome when stress perfusion CMR is assessed visually side-by-side with LGE, as per guidelines[11] and as in our study. Nevertheless, rest perfusion imaging remains a fundamental requirement for perfusion guantification and MPR estimation.

509

510 Semi-automated quantitative assessment performed better than Level-1 and511 Level-2 operators and similarly to Level-3 operators for the detection of

512 CAD. The latter is in keeping with the results of several other studies that 513 reported high sensitivity and specificity for quantitative analysis, with 514 sensitivity ranging from 80%[22] to 94.4%[32] and specificity ranging from 515 81%[33] to 100%[34]. Previous studies from Patel et al[6] and Mordini et 516 al[35] compared quantitative with visual and semi-quantitative analysis and 517 demonstrated that quantitative analysis is superior to visual assessment and 518 semi-quantitative assessment in the detection of ischemia, and that 519 quantitative analysis is the most accurate method to measure the total 520 ischemic burden.

521 In the present study, quantitative analysis was performed using a semi-522 automated method which requires user input to confirm the automated 523 segmentation of the images but eliminates inter-observer variability for 524 what concerns the quantification procedure. This is of increasing relevance 525 as recent technical advances in image reconstruction and analysis 526 techniques are likely to permit the clinical translation of robust and fully 527 automated quantitative analysis into routine clinical practice [36-39]. In our 528 study however, the dual bolus approach used for arterial input function 529 measurements failed in 2 subjects, impeding quantitative analysis. The 530 advent of dual sequences capable of a more accurate assessment of the 531 concentration of gadolinium in the main bolus input function may make the 532 use of dual bolus redundant in the near future[37,40].

533

#### 534 Limitations

535 This study included a selected population with suspected CAD and we 536 excluded patients with primary cardiomyopathy. Thus, our results on

537 diagnostic accuracy do not include other patterns of perfusion
538 abnormalities, which may require even more experience to discern (e.g.,
539 microvascular dysfunction).

540 Moreover, we used an anatomical reference standard (invasive coronary 541 angiography) to compare operators' performances in interpreting a 542 functional test, while a functional reference standard (e.g., fractional flow 543 reserve) may be more appropriate.

544 Our results demonstrate that similarly accurate detection of CAD can be 545 achieved by Level-3 operators and by automated perfusion quantification. 546 Although our study was not powered to demonstrate the superiority of 547 quantitative analysis, this has been the subject of a recent study which has 548 reported very similar findings[30]. The non-inferiority of automated 549 quantification to expert visual reads, in combination with the prognostic 550 value of quantitative analysis<sup>[23]</sup> will facilitate more widespread adoption 551 of stress perfusion CMR by less experienced readers.

Finally, all stress perfusion CMR were acquired in a single center, using a 3T
Philips scanner and a high-resolution k-t sequence. This may not reflect the
standard clinical acquisition in other centres.

555

# 556 <u>Conclusions</u>

557 This study demonstrates that visual assessment of stress perfusion CMR is 558 challenging for Level-1 and Level-2 operators but accurate in the hands of 559 Level-3 operators. Our results highlight the importance of the 560 recommendations of the ESC/EACVI training guidelines in CMR, which 561 recommend independent reporting for Level-3 operators only and

562 supervised reporting for Level-2 trained operators. The availability of rest 563 perfusion images was associated with significantly higher confidence and 564 higher perceived image quality, regardless of the level of training of the 565 operator. Quantitative analysis performed similarly to Level-3 trained 566 operators and could represent, in the future, a valid alternative to visual 567 assessment.

568

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583

584 **Declarations** 

585 Ethics approval and consent to participate: All subjects gave written
586 informed consent in accordance with ethical approval (ethics 15/NS/0030,
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588 **Consent for publication**: Not applicable.

589 Availability of data and materials: Please contact author for data requests.

590 Competing interests: The authors declare that they have no competing591 interests.

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Authors' contribution: ADMV, LC, NB and AC conceived the study and participated in the study design and coordination. IN, GDG, NC, CF, MSN, JK, ES, VDF and AS analysed the data. ADMV, LC, XM, CS and TFI performed the data analysis. AC segmented the data for quantitative analysis. ADMV and LC drafted the manuscript. All authors critically revised the manuscript for important intellectual content, read and approved the final manuscript.

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# 611 **<u>References</u>**

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612 1. Task Force Members, Montalescot G, Sechtem U, Andreotti F, Arden C, 613 Budaj A, et al. 2013 ESC guidelines on the management of stable coronary 614 artery disease: The Task Force on the management of stable coronary artery 615 disease of the European Society of Cardiology. European Heart Journal. 616 2013;34:2949-3003. 617 2. Authors Task Force members, Kolh P, Alfonso F, Collet J-P, Cremer J, Falk V, et al. 2014 ESC/EACTS Guidelines on myocardial revascularization. 618 619 European Heart Journal. The Oxford University Press; 2014;35:ehu278-619. 620 3. Schwitter J, Wacker CM, Wilke N, Al-Saadi N, Sauer E, Huettle K, et al. Superior diagnostic performance of perfusion-cardiovascular magnetic 621 622 resonance versus SPECT to detect coronary artery disease: The secondary 623 endpoints of the multicenter multivendor MR-IMPACT II (Magnetic 624 Resonance Imaging for Myocardial Perfusion Assessment in Coronary Artery 625 Disease Trial). J Cardiovasc Magn Reson. Journal of Cardiovascular Magnetic 626 Resonance; 2012;14:1-1. 627 4. Nandalur KR, Dwamena BA, Choudhri AF, Nandalur MR, Carlos RC. 628 Diagnostic Performance of Stress Cardiac Magnetic Resonance Imaging in 629 the Detection of Coronary Artery Disease. J Am Coll Cardiol. 2007;50:1343-630 53. 631 5. Li M, Zhou T, Yang L-F, Peng Z-H, Ding J, Sun G. Diagnostic accuracy of 632 myocardial magnetic resonance perfusion to diagnose ischemic stenosis 633 with fractional flow reserve as reference: systematic review and meta-634 analysis. JACC: Cardiovascular Imaging. 2014;7:1098-105. 635 6. Patel AR, Antkowiak PF, Nandalur KR, West AM, Salerno M, Arora V, et al. 636 Assessment of advanced coronary artery disease: advantages of quantitative 637 cardiac magnetic resonance perfusion analysis. J Am Coll Cardiol. 638 2010;56:561-9. 639 7. Ferreira PF, Gatehouse PD, Mohiaddin RH, Firmin DN. Cardiovascular 640 magnetic resonance artefacts. J Cardiovasc Magn Reson. 2013;15:41. 641 8. Chiribiri A, Leuzzi S, Conte MR, Bongioanni S, Bratis K, Olivotti L, et al. Rest 642 perfusion abnormalities in hypertrophic cardiomyopathy: correlation with 643 myocardial fibrosis and risk factors for sudden cardiac death. Clinical 644 Radiology. 2015;70:495-501. 645 9. Villa ADM, Sammut E, Zarinabad N, Carr-White G, Lee J, Bettencourt N, et 646 al. Microvascular ischemia in hypertrophic cardiomyopathy: new insights from high-resolution combined quantification of perfusion and late 647 648 gadolinium enhancement. J Cardiovasc Magn Reson. 2016;18:4.

- 649 10. Klem I, Heitner JF, Shah DJ, Sketch MH, Behar V, Weinsaft J, et al.
- 650 Improved detection of coronary artery disease by stress perfusion
- 651 cardiovascular magnetic resonance with the use of delayed enhancement
- infarction imaging. J Am Coll Cardiol. 2006;47:1630–8.
- 653 11. Schulz-Menger J, Bluemke DA, Bremerich J, Flamm SD, Fogel MA,
- Friedrich MG, et al. Standardized image interpretation and post processing
- 655 in cardiovascular magnetic resonance: Society for Cardiovascular Magnetic
- 656 Resonance (SCMR) Board of Trustees Task Force on Standardized Post
- 657 Processing. J Cardiovasc Magn Reson. BioMed Central Ltd; 2013;15:35.
- 12. Plein S, Schulz-Menger J, Almeida A, Mahrholdt H, Rademakers F, Pennell
- D, et al. Training and accreditation in cardiovascular magnetic resonance in
- 660 Europe: a position statement of the working group on cardiovascular
- 661 magnetic resonance of the European Society of Cardiology. European Heart
- 662Journal. Oxford University Press; 2011;32:793–8.
- 663 13. Ishida M, Schuster A, Morton G, Chiribiri A, Hussain ST, Paul M, et al.
- 664 Development of a universal dual-bolus injection scheme for the quantitative
- assessment of myocardial perfusion cardiovascular magnetic resonance. J
- 666 Cardiovasc Magnetic Resonance. 2011;13:28.
- 667 14. Cerqueira MD, Weissman NJ, Dilsizian V, Jacobs AK, Kaul S, Laskey WK, et
- al. Standardized Myocardial Segmentation and Nomenclature for
- 669 Tomographic Imaging of the Heart A Statement for Healthcare Professionals
- 670 From the Cardiac Imaging Committee of the Council on Clinical Cardiology of
- 671 the American Heart Association. Int J Cardiovasc Imaging [Internet].
- 672 Lippincott Williams & Wilkins; 2002;18:539–42. Available from:
- 673 http://circ.ahajournals.org/cgi/doi/10.1161/hc0402.102975
- 15. Kramer CM, Barkhausen J, Flamm SD, Kim RJ, Nagel E. Standardized
- 675 cardiovascular magnetic resonance (CMR) protocols 2013 update. J
- 676 Cardiovasc Magnetic Resonance. 2013;15:91.
- 677 16. Kim RJ, Wu E, Rafael A, Chen E-L, Parker MA, Simonetti O, et al. The Use
- 678 of Contrast-Enhanced Magnetic Resonance Imaging to Identify Reversible 670 Muccardial Ducting tion N Engl I Med 2000;242:1445 52
- 679 Myocardial Dysfunction. N Engl J Med. 2000;343:1445–53.
- 680 17. Hautvast G, Chiribiri A, Zarinabad N, Schuster A, Breeuwer M, Nagel E.
- 681 Myocardial blood flow quantification from MRI by deconvolution using an
- exponential approximation basis. IEEE Trans Biomed Eng. 2012;59:2060–7.
- 683 18. Wilke N, Jerosch-Herold M, Wang Y, Huang Y, Christensen BV, Stillman
- AE, et al. Myocardial perfusion reserve: assessment with multisection,
- 685 quantitative, first-pass MR imaging. Radiology. 1997;204:373–84.
- 686 19. Jerosch-Herold M, Wilke N, Stillman AE. Magnetic resonance
- 687 quantification of the myocardial perfusion reserve with a Fermi function
- 688 model for constrained deconvolution. Med Phys. 1998;25:73–84.

- 689 20. Zarinabad N, Chiribiri A, Hautvast GLTF, Ishida M, Schuster A, Cvetkovic
- 690 Z, et al. Voxel-wise quantification of myocardial perfusion by cardiac
- 691 magnetic resonance. Feasibility and methods comparison. Magnetic
- 692 Resonance in Medicine. 2012;68:1994–2004.
- 693 21. Sammut E, Zarinabad N, Wesolowski R, Morton G, Chen Z, Sohal M, et al.
- 694 Feasibility of high-resolution quantitative perfusion analysis in patients with 695 heart failure 1 Cardiovasc Magn Peson, 2015:17:12
- heart failure. J Cardiovasc Magn Reson. 2015;17:13.
- 696 22. Lockie T, Ishida M, Perera D, Chiribiri A, De Silva K, Kozerke S, et al. High-
- 697 resolution magnetic resonance myocardial perfusion imaging at 3.0-Tesla to
- 698 detect hemodynamically significant coronary stenoses as determined by
- 699 fractional flow reserve. J Am Coll Cardiol. 2011;57:70–5.
- 700 23. Sammut EC, Villa ADM, Di Giovine G, Dancy L, Bosio F, Gibbs T, et al.
- 701 Prognostic Value of Quantitative Stress Perfusion Cardiac Magnetic
- 702 Resonance. JACC: Cardiovascular Imaging. 2017.
- 703 24. Fihn SD, Gardin JM, Abrams J, Berra K, Blankenship JC, Dallas AP, et al.
- 704 2012 ACCF/AHA/ACP/AATS/PCNA/SCAI/STS guideline for the diagnosis
- and management of patients with stable ischemic heart disease: a report of
- the American College of Cardiology Foundation/American Heart Association
- task force on practice guidelines, and the American College of Physicians,
- 708 American Association for Thoracic Surgery, Preventive Cardiovascular
- 709 Nurses Association, Society for Cardiovascular Angiography and
- 710 Interventions, and Society of Thoracic Surgeons. Circulation. 2012. pp. e354–
- 711 471.
- 712 25. American College of Cardiology Foundation Task Force on Expert
- 713 Consensus Documents, Hundley WG, Bluemke DA, Finn JP, Flamm SD, Fogel
- 714 MA, et al. ACCF/ACR/AHA/NASCI/SCMR 2010 expert consensus document
- on cardiovascular magnetic resonance: a report of the American College of
- 716 Cardiology Foundation Task Force on Expert Consensus Documents.
- 717 Circulation. 2010. pp. 2462–508.
- 718 26. Greenwood JP, Maredia N, Younger JF, Brown JM, Nixon J, Everett CC, et
- al. Cardiovascular magnetic resonance and single-photon emission
- 720 computed tomography for diagnosis of coronary heart disease (CE-MARC): a
- 721 prospective trial. The Lancet. 2012;379:453–60.
- 722 27. Schwitter J, Wacker CM, Wilke N, Al-Saadi N, Sauer E, Huettle K, et al. MR-
- 723 IMPACT II: Magnetic Resonance Imaging for Myocardial Perfusion
- Assessment in Coronary artery disease Trial: perfusion-cardiac magnetic
- resonance vs. single-photon emission computed tomography for the
- 726 detection of coronary artery disease: a comparative multicentre,
- multivendor trial. European Heart Journal. 2013;34:775–81.
- 728 28. Patel MR, Peterson ED, Dai D, Brennan JM, Redberg RF, Anderson HV, et
- al. Low diagnostic yield of elective coronary angiography. N Engl J Med.
- 730 Massachusetts Medical Society; 2010;362:886–95.

- 731 29. Kim RJ, De Roos A, Fleck E, Higgins CB, Pohost GM, Prince M, et al.
- 732 Guidelines for training in Cardiovascular Magnetic Resonance (CMR). J
- 733 Cardiovasc Magn Reson. 2007. pp. 3–4.
- 30. Biglands JD, Ibraheem M, Magee DR, Radjenovic A, Plein S, Greenwood JP.
- 735 Quantitative Myocardial Perfusion Imaging Versus Visual Analysis in
- 736 Diagnosing Myocardial Ischemia: A CE-MARC Substudy. JACC:
- 737 Cardiovascular Imaging. JACC: Cardiovascular Imaging; 2018;11:711–8.
- 738 31. Kruger J, Dunning D. Unskilled and unaware of it: how difficulties in
- recognizing one's own incompetence lead to inflated self-assessments. J Pers
  Soc Psychol. 1999;77:1121–34.
- 741 32. Biglands JD, Magee DR, Sourbron SP, Plein S, Greenwood JP, Radjenovic
- A. Comparison of the Diagnostic Performance of Four Quantitative
- 743 Myocardial Perfusion Estimation Methods Used in Cardiac MR Imaging: CE-
- 744 MARC Substudy. Radiology. Radiological Society of North America;
- 745 2015;275:393-402.
- 746 33. Morton G, Chiribiri A, Ishida M, Hussain ST, Schuster A, Indermuehle A, et
- al. Quantification of Absolute Myocardial Perfusion in Patients With
- 748 Coronary Artery Disease: Comparison Between Cardiovascular Magnetic
- 749 Resonance and Positron Emission Tomography. J Am Coll Cardiol. Journal of
- the American College of Cardiology; 2012;60:1546–55.
- 751 34. Bernhardt P, Walcher T, Rottbauer W, Wöhrle J. Quantification of
- myocardial perfusion reserve at 1.5 and 3.0 Tesla: a comparison to fractional
- 753 flow reserve. Int J Cardiovasc Imaging. 2012;28:2049–56.
- 754 35. Mordini FE, Haddad T, Hsu LY, Kellman P, Lowrey TB, Aletras AH, et al.
- 755 Diagnostic accuracy of stress perfusion CMR in comparison with quantitative
- coronary angiography: fully quantitative, semiquantitative, and qualitative
- assessment. JACC: Cardiovascular Imaging. 2014;7:14–22.
- 758 36. Zarinabad N, Hautvast GLTF, Sammut E, Arujuna A, Breeuwer M, Nagel E,
- et al. Effects of Tracer Arrival Time on the Accuracy of High-Resolution
- 760 (Voxel-Wise) Myocardial Perfusion Maps from Contrast-Enhanced First-Pass
- 761 Perfusion Magnetic Resonance. Biomedical Engineering, IEEE Transactions
- 762 on. IEEE; 2014;61:2499–506.
- 763 37. Kellman P, Hansen MS, Nielles Vallespin S, Nickander J, Themudo R,
- 764 Ugander M, et al. Myocardial perfusion cardiovascular magnetic resonance:
- 765 optimized dual sequence and reconstruction for quantification. J Cardiovasc766 Magn Reson. 2017;19:43.
- 767 38. Jacobs M, Benovoy M, Chang L-C, Arai AE, Hsu LY. Evaluation of an
- 768 automated method for arterial input function detection for first-pass
- 769 myocardial perfusion cardiovascular magnetic resonance. J Cardiovasc Magn
- 770 Reson. 2016;18:17.

- 39. Hsu LY, Jacobs M, Benovoy M, Ta AD, Conn HM, Winkler S, et al.
- 772 Diagnostic Performance of Fully Automated Pixel-Wise Quantitative
- 773 Myocardial Perfusion Imaging by Cardiovascular Magnetic Resonance. JACC:
- Cardiovascular Imaging. JACC: Cardiovascular Imaging; 2018;11:697–707.
- 40. Gatehouse P, Lyne J, Smith G, Pennell D, Firmin D. T2\* effects in the dual-
- sequence method for high-dose first-pass myocardial perfusion. Journal of
- 777 Magnetic Resonance Imaging. 2006;24:1168–71.
- 778

#### 779 Figure titles and legends

- 780 **Figure 1**. Study flowchart.
- 781 CMR: cardiovascular magnetic resonance, LGE: late gadolinium
- 782 enhancement.
- 783
- **Figure 2**. Percentage of correct coronary artery disease (CAD) identification
- 785 (diagnostic accuracy) for different levels of CMR training and using
- 786 quantitative assessment.
- 787 CAD: coronary artery disease, CMR: cardiovascular magnetic resonance.
- 788
- **Figure 3**. Percentage of correct CAD identification (diagnostic accuracy)
- 790 stratified by coronary territory.
- 791 CAD: coronary artery disease, LAD: left anterior descending coronary artery,
- 792 LCX: left circumflex coronary artery, RCA: right coronary artery.
- 793
- 794 **Figure 4**. Sensitivity and specificity for level of CMR training. \* denotes
- statistically significant difference (p< 0.001) between sensitivity values. \*\*
- denotes statistically significant difference (p< 0.001) between specificity
- 797 values.
- 798 Sens: sensitivity, spec: specificity.
- 799
- 800 **Figure 5**. Percentage of correct identification of CAD (diagnostic accuracy)
- 801 using stress perfusion only or stress and rest images.
- 802 CAD: coronary artery disease.
- 803

- 804 **Figure 6**. CAD classification for different levels of CMR training.
- 805 CAD: coronary artery disease, 1VD: one-vessel disease, 2VD, two-vessel
- 806 disease, 3VD: three-vessel disease.