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Citation for published version (APA):

Nettis, M. A., Veronese, M., Nikkheslat, N., Lombardo, G., Mariani, N., Sforzini, L., Enache, D., Harrison, N. A., Turkheimer, F., Mondelli, V., & Pariante, C. (2020). PET imaging shows no changes in TSPO brain density after IFN- α immune challenge 4 in healthy human volunteers. *Translational psychiatry*.

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3 **PET imaging shows no changes in TSPO brain density after IFN- α immune challenge**
4 **in healthy human volunteers**

5

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34 Running title: TSPO imaging in healthy humans following IFN- α challenge

35

36 **Abstract**

37

38 Depression is associated with peripheral inflammation, but its link with brain microglial
39 activity remains unclear. In seven healthy males, we used repeated translocator protein-
40 Positron Emission Tomography (TSPO-PET) dynamic scans with [¹¹C]PBR28 to image
41 brain microglial activation before and 24 hours after the immune challenge interferon (IFN)-
42 α . We also investigated the association between changes in peripheral inflammation,
43 changes in microglial activity, and changes in mood. IFN- α administration decreased
44 [¹¹C]PBR28 PET tissue volume of distribution (Vt) across the brain (-20 \pm 4%; t_6 =4.1,
45 p =0.01), but after correction for radioligand free-plasma fraction there were no longer any
46 changes (+23 \pm 31%; t =0.1, p =0.91). IFN- α increased serum IL-6 (1826 \pm 513%, t_6 =-7.5,
47 p <0.001), IL-7 (39 \pm 12%, t_6 =-3.6, p =0.01), IL-10 (328 \pm 48%, t_6 =-12.8, p <0.001) and IFN- γ
48 (272 \pm 64%, t_6 =-7.0, p <0.001) at 4-6 hours, and increased serum TNF- α (49 \pm 7.6%, t_6 =-7.5,
49 p <0.001), IL-8 (39 \pm 12%, t_6 =-3.5, p =0.013) and C-reactive protein (1320 \pm 459%, t_6 =-7.2,
50 p <0.001) at 24 hours. IFN- α induced temporary mood changes and sickness symptoms
51 after 4-6 hours, measured as an increase in POMS-2 total mood score, confusion and
52 fatigue, and a decrease in vigor and friendliness (all p \leq 0.04). No association was found
53 between changes in peripheral inflammation and changes in PET or mood measures. Our
54 work suggests that brain TSPO-PET signal is highly dependent of inflammation-induced
55 changes in ligand binding to plasma proteins. This limits its usefulness as a sensitive
56 marker of neuroinflammation and consequently, data interpretation. Thus, our results can be
57 interpreted as showing either that [¹¹C]PBR28 is not sensitive enough under these
58 conditions, or that there is simply no microglial activation in this model.

59

60

61 **Introduction**

62

63 Microglial activation has been proposed as the core neuroinflammatory process in
64 psychiatric disorders. Microglia are brain resident macrophages and the primary immune
65 effector cells in the central nervous system. Previous preclinical and post-mortem studies
66 investigating the role of inflammation in depression have shown an association between
67 depressive symptoms and greater microglial activity (1-4), suggesting that the brain's innate
68 immune response might play a role in the pathophysiology of depression. In vivo, microglial
69 activation can be measured with positron emission tomography (PET) radioligands
70 targeting translocator protein (TSPO), a protein located on outer mitochondrial membranes
71 in microglia, as TSPO appears to be overexpressed when microglial cells are activated
72 during neuroinflammation (5).

73

74 Despite some negative results (6), the majority of TSPO-PET studies in patients with
75 depression have reported increased TSPO binding compared with healthy controls (7-11),
76 suggesting increased microglial activation in these patients. These studies thus propose
77 that the inflammatory response in depression involves not only the periphery (12) (13) but
78 also the brain. Indeed, behavioural symptoms of depression might be induced by peripheral
79 cytokines and immune cells acting on the brain to elicit a neuroinflammatory response (14,
80 15). However, no PET study so far has found a correlation between peripheral and central
81 inflammatory markers in patients with depression, and so the mechanism underpinning
82 these co-existing findings remains unclear (4). Moreover, a recent meta-analysis from our
83 team (4) has highlighted the heterogeneity of these PET studies in terms of study design,
84 methods and selected sample. For example, studies using first generation radiotracers
85 used the binding potential as endpoint, which is calculated by normalizing the activity in the

86 target region with the activity of a region devoid of TSPO; since TSPO is ubiquitous, in this
87 case normalization is achieved by a pseudo-reference region with a kinetic profile similar to
88 the one measured in healthy controls (16). The quantification of second generation tracers,
89 instead, mostly uses the volume of distribution as endpoint, which is the estimated ratio at
90 equilibrium between the activity in the target and the activity in plasma (16).

91

92 Of note, there are also quite a lot of differences between these studies in depression. For
93 example, and of particular relevance to the present study, only two studies (6) (11)
94 corrected for the free-plasma fraction of the ligand, that is, how much of the ligand is
95 available for brain tissue binding as it is not bound to plasma proteins, which is important
96 given the evidence of TSPO ligand binding to peripheral inflammatory proteins (17).
97 Moreover, studies included depressed patients with different ages (including late-life
98 depression (8)), symptoms severity and medication status (18), and only three examined
99 drug-free depressed patients (9-11).

100

101 Considering the intrinsic clinical heterogeneity of the depressed clinical population, studies
102 in healthy volunteers are important to dissect the mechanisms linking peripheral and central
103 inflammation. Experimental models in animals have demonstrated that microglial activation
104 can be induced by a peripheral immune challenge; for example, many studies have used
105 *Escherichia coli* lipopolysaccharide (LPS) as peripheral immune challenge to elicit
106 microglial activation in rodents (19, 20). In line with this evidence, two TSPO-PET studies
107 have investigated non-human primates following LPS administration, and both showed a
108 significant increase in TSPO [¹¹C]PBR28 binding in the brain (21, 22). Moreover, the study
109 by Hannestad and colleagues also found correlations between peripheral cytokines levels
110 and the TSPO binding. So far, only one PET study (also with [¹¹C]PBR28) has used LPS in

111 humans, in eight healthy males, finding increased TSPO binding (by 30–60%) after 3 hours
112 from the LPS injection, although TSPO binding did not correlate with peripheral
113 inflammation nor with measures of mood (23).

114

115 In the present study, we examine peripherally-induced systemic inflammation and brain
116 TSPO binding in healthy humans using interferon (IFN)- α (24, 25). IFN- α is a pro-
117 inflammatory cytokine with antiviral, anticancer, and immunomodulatory effects, approved
118 for treatment of cancer and chronic hepatitis C (26, 27). IFN- α induces a systemic immune
119 response associated with sickness behavior, and, when administered over weeks or
120 months as a treatment for patients with cancer or hepatitis C, is associated with a diagnosis
121 of major depression in up to 30-50% of patients, and is thus considered the most validated
122 clinical model of inflammation-induced depression (28). Supporting our choice of using this
123 model, preclinical studies have shown that peripheral IFN- α treatment in mice induces
124 activation of microglia, and that this activation is associated with depressive-like behavior
125 (29, 30).

126

127 Similarly to the aforementioned LPS study in humans (23), here we measure microglial
128 activation with [^{11}C]PBR28 PET, before, and 24 hours after a single IFN- α administration,
129 in seven healthy male subjects. Of note, second generation ligands, such as [^{11}C]PBR28,
130 show a higher signal-to-noise ratio compared with first generation ones, facilitating
131 measurement of significant within-subjects changes with a smaller sample size (5).
132 However, their binding affinity depends on the rs6971 nucleotide polymorphism on the
133 TSPO gene (31), and the quantification of the brain signal is confounded by the presence of
134 abundant TSPO in endothelial cells and by the high ligand affinity for plasma proteins (32).
135 Here we apply a quantification methodology that takes into account all these limitations –

136 something which the previous LPS study did not do. The decision to have the second PET
137 scan 24 hours after the IFN- α administration was based on pre-clinical studies showing that
138 in vitro IFN- α -stimulated microglia releases inflammatory cytokines after approximately 24
139 hours (33). We also measure the levels of peripheral cytokines and the transient changes in
140 mood after IFN- α . Based on the evidence discussed above, we hypothesize that the IFN- α
141 injection would induce an increase in brain TSPO binding, in peripheral inflammation and in
142 depressive-like symptoms, with possible correlations between these three sets of variables.

143

144

145 **Materials and Methods**

146

147 Subjects: Seven healthy males provided written informed consent and participated in the
148 study. This study was approved by the Queen Square London Ethical committee, ref.
149 16/LO/1520. Participants were recruited through King's College London internal e-mail,
150 online platforms and public advertising. In order to determine eligibility, participants had a
151 pre-screening phone call, followed by a screening visit. Their medical history was collected,
152 and a MINI Psychiatric scale administered. Eligible participants were non-smokers, drank no
153 more than 5 alcohol drinks per week, had no history of significant medical illness and did
154 not meet the criteria for any current or past psychiatric or substance-dependence diagnosis.
155 Subjects were excluded if they had had an infection in the last month or had regularly used
156 anti-inflammatory drugs. Subjects were also instructed to abstain from alcohol, anti-
157 inflammatory medication and physical exercise for 72 hours before the scans. During the
158 screening visit, participants were genotyped for the rs6971 polymorphism on the TSPO
159 gene. Only high-affinity binders (HABs) of [^{11}C]PBR28 were included (see Table 1 for main
160 sociodemographic features).

161

162 **TABLE 1 around here**

163

164 Study design: Each participant was assessed four times: at a Screening Visit, to evaluate
165 their eligibility; at Visit 1, when we collected the baseline venous blood sample to measure
166 C-reactive protein (CRP) as a peripheral inflammatory marker, and participants had their
167 *first* (baseline) PET scan; at Visit 2, when IFN- α was administered, and serum peripheral
168 biomarkers (CRP and cytokines) and clinical symptoms were measured 1 hour before, and
169 at 2, 4 and 6 hours after the injection; and at Visit 3, 24 hours after the administration of
170 IFN- α , when serum peripheral biomarkers (CRP and cytokines) and clinical symptoms were
171 again assessed, and participants had their *second* PET scan (see Figure 1 for a summary
172 of the study design).

173

174 The two [^{11}C]PBR28 PET scans lasted 90 min each, with 7 or 8 days between the 2 scans
175 for most patients (that is, Visit 1 and Visit 3), although two participants had the second
176 scans 1 and 6 months after the first, but always 24 hours after the IFN- α injection (that is,
177 Visit 3 was always 24 hours after Visit 2) (Fig. 1). To minimise intra and inter-subject
178 variability, and limiting the effects of circadian rhythm on TSPO density (34, 35), all scans
179 were conducted between 13:00 and 15:30, and within each individual both scans were
180 conducted at *exactly* the same time (Table 1, Supplemental Material). All subjects
181 underwent high-resolution T1 magnetic resonance imaging (MRI), before IFN- α
182 administration, in a Siemens Tim Trio 3T scanner (Siemens healthcare, Erlangen,
183 Germany); these structural MRI images were co-registered with the PET imaging to identify
184 the anatomical regions of interest. All experimental variables related to PET imaging
185 acquisition are described in Supplemental Materials.

186

187 **FIGURE 1 around here**

188

189 IFN- α administration: At visit 2, participants received a subcutaneous injection of IFN- α 2a
190 (Roferon-A 3 million IU/0.5 ml solution for injection). We monitored vital signs (heart rate,
191 blood pressure, temperature) and the occurrence of adverse effects every hour for 8 hours
192 after the injection. Participants were allowed to take 1 gr of paracetamol, once or twice, if
193 sickness symptoms were difficult to tolerate, and 6 out of the 7 participants did so.

194

195 PET imaging: an initial low-dose computer tomography (CT) scan was acquired for
196 attenuation and scatter correction using Siemens Biograph™ True Point™ PET/CT scanner
197 (Siemens Medical Systems, Germany). Subjects then received a bolus injection of
198 [^{11}C]PBR28 (target dose \sim 300 Mbq) followed by a 90-min PET emission scan. PET data
199 were acquired in 3D mode and binned into 26 frames (durations: 8×15 s, 3×1 min,
200 5×2 min, 5×5 min, 5×10 min). Images were reconstructed using filtered back projection
201 and corrected for attenuation and scatter. Radiopharmaceutical preparation acquisition
202 protocol were consistent with previous studies (36-38).

203

204 In parallel to the PET acquisition, arterial blood was sampled from the radial artery using a
205 combined automatic and manual approach. A continuous sampling system (ABSS Allogg,
206 Mariefred, Sweden) was used to measure whole blood activity for the first 15 min of each
207 scan at the rate of one sample per second. Discrete blood samples were manually taken at
208 5, 10, 15, 20, 25, 30, 40, 50, 60, 70, 80, 90 min, centrifuged and used to determine the
209 plasma over blood activity ratio (POB). Samples at 5, 10 and 15 min were used to calibrate
210 the two sampling modalities. Samples taken at 5, 10, 20, 30, 50, 70 and 90 min were also

211 analysed using radio-high performance liquid chromatography (HPLC) to calculate the
212 plasma fraction of ligand free of metabolites (PPf). Radiometabolite analysis of [¹¹C]PBR28
213 in the blood was done as described previously (36). Ligand free plasma fraction (fp), or the
214 portion of [¹¹C]PBR28 unbound to plasma proteins, was determined for all scans using
215 ultrafiltration-based method as previously described (6).

216

217 Imaging analysis: Structural MRI images were used for grey/white matter segmentation and
218 region of interest (ROI) definition. A neuroanatomical atlas was co-registered on each
219 subject's MRI scan and PET image using a combination of Statistical Parametric Mapping 8
220 (<http://www.fil.ion.ucl.ac.uk/spm>) and FSL (<http://www.fsl.fmrib.ox.ac.uk/fsl>) functions,
221 implemented in MIAKAT™ (<http://www.imanova.co.uk>). ROIs included occipital lobe,
222 temporal lobe, frontal lobe, parietal lobe, insular cortex, cingulate cortex, amygdala,
223 hippocampus, thalamus, striatum and cerebellum. All PET images were corrected for head
224 movement using non-attenuation-corrected images as they include greater scalp signal,
225 which improves re-alignment compared to attenuation-corrected images. Frames were
226 realigned to a single "reference" space identified by the PET frame with the highest activity.
227 The transformation parameters were then applied to the corresponding attenuation-
228 corrected PET frames to create a movement-corrected dynamic image for analysis.
229 Regional tissue-time activity curves (TACs) were obtained by sampling the image with the
230 co-registered atlas.

231

232 Arterial blood data processing: Processing of blood samples was performed consistently
233 with previous studies (36). Both POB and PPf were fitted with an extended Hill model
234 (39) that provided the best data description (40). Whole blood TACs were fitted using a
235 variation of Feng's model that consists in a straight line to the arterial input function peak

236 followed by a tri-exponential decay (41). For each scan, the difference between ligand
237 arrival time in the brain and arterial sampling site was estimated by shifting blood curves 0-
238 20s (both parent and whole blood TACs), fitting the whole brain TAC (using exponential
239 spectral analysis to avoid dependency on a particular compartmental model), and selecting
240 the delay that produced the smallest weighted residual sum of squares.

241

242 Kinetic analysis: Quantification of [¹¹C]PBR28 tissue distribution was performed using both
243 the standard 2TCM and the 2TCM-1K with total distribution volume (Vt) as main parameter
244 of interest (42). The two models were then used to assess Vt changes before and after IFN-
245 α (% Δ Vt), as done in a previous study (43).

246

247 Biomarkers of peripheral inflammation: At Visit 1 (baseline), a blood sample was collected
248 for the first CRP analysis at the time of the first PET scan. At Visit 2, blood samples were
249 taken 1 hour before IFN- α injection, and at 2, 4, and 6 hours after IFN- α injection, and then,
250 at Visit 3, at 24 hours after IFN- α injection, to measure CRP and other immune biomarkers,
251 based on previous work by Cassidy et al. (44) (Fig. 1). Serum high sensitivity C-reactive
252 protein (hsCRP) was assayed on the Siemens Advia 2400 Chemistry analyser (Siemens
253 Healthcare Diagnostics, Frimley, UK) (45). Serum cytokines were measured using Meso
254 Scale Discovery (MSD) V-PLEX sandwich immunoassays (46, 47), and plates read on an
255 MSD QuickPlex SQ 120, as in a previous study conducted in our laboratory (48, 49). MSD
256 Pro-inflammatory Panel 1 (human) kit was used for the measurement of IFN- γ , IL-1 β , IL-2,
257 IL-4, IL-6, IL-8, IL-10, IL-12p70, IL-13, and TNF- α , and a custom Cytokine Panel 1 (human)
258 kit was used for the measurement of IL-7, IL-17 A and vascular endothelial growth factor
259 VEGF-A. The inter-assay coefficient of variations was <10%. The results were analysed
260 using MSD DISCOVERY WORKBENCH analysis software. Finally, levels of serum S100B

261 protein were measured in serum as a marker of blood–brain barrier (BBB) permeability
262 (50, 51), using a S100B kit distributed by Diasorin, Charles House, Toutley Road,
263 Wokingham, Berkshire, run on the Liaison XL chemiluminescence analyser (52, 53).

264

265 We measured levels of tryptophan, kynurenine and kynurenine pathway metabolites, 3-
266 hydroxykynurenine and kynurenic acid (54, 55) using automated on-line solid-phase
267 extraction HPLC-tandem mass spectrometry (see Supplemental Materials).

268

269 Clinical symptoms: The Mini International Neuropsychiatric Interview (MINI) was used at
270 Screening Visit to diagnose a previous history of psychiatric disorders (56). At all
271 timepoints, from Visit 1 to Visit 3, the Profile of Mood States (POMS-2) and the State
272 Anxiety Inventory (STAI-S) were administered to assess how participants were feeling “right
273 now”. These are self-administered tool which allows to easily test-retest affect states and
274 sickness symptoms (57) (58). In particular, POMS and STAI-S have already been used in
275 studies assessing behavioural symptoms following IFN- α (59) and LPS injection (60).

276

277 Statistical analysis: We performed two-tailed, paired t-tests with $p < 0.05$ to investigate
278 differences in [^{11}C]PBR28 signal between baseline and IFN- α challenge (~24 hours after
279 the injection). V_t values showed a normal distribution in both 2TCM and 2TCM-K1 models,
280 before and after fp correction (all $p > 0.5$ with the Shapiro-Wilk test). Changes in cytokines
281 and clinical measures were analysed using repeated measures ANOVA followed by paired
282 t-test comparing baseline values (1 hour before IFN- α) with those at 2, 4, 6 and 24 hours.
283 Correlation analyses were performed to test the association between changes in V_t and
284 changes in cytokines levels and in clinical symptoms scores. While clinical symptoms

285 scores were normally distributed, cytokines values were not, so we applied a logarithmic
286 transformation. All data are presented as mean and standard errors of the mean.

287

288

289 **Results**

290

291 *Measured [¹¹C]PBR28 PET uptake is influenced by inflammation-induced changes in the*
292 *free plasma fraction of the radio ligand, and there are no IFN- α effects once adjusted for*
293 *this*

294

295 The administration of IFN- α led to a generalized reduction of [¹¹C]PBR28 PET uptake
296 across the entire brain in all subjects but one (Fig. 2A, lower part). Between baseline and
297 24 hours after the challenge, the 2TCM model showed a whole brain mean signal reduction
298 ($\% \Delta V_t$ mean \pm SE) of $-20 \pm 4\%$ (paired t-test $t = -4.18$, $p = 0.01$), with only one participant
299 showing a 2% increase. The other regions of interest showed a similar pattern of reduction,
300 ranging from -14% for the Amygdala, to -26% for the Insular cortex (Fig. 2A, upper part).

301

302 Interestingly, 77% of this change in V_t between the two scans was caused by a change in
303 tracer blood-to-tissue transport (K_1), suggesting a reduced availability of ligand blood flow
304 to the brain. In order to examine whether this reduced availability might be related to the
305 ligand binding to plasma proteins, we further analyzed the ligand free plasma fraction (f_p)
306 and its effect on the arterial blood and plasma [¹¹C]PBR28 activity. Indeed, the f_p
307 decreased significantly in the second scan, ($\% \Delta f_p = -18 \pm 16\%$, mixed effects modelling $z = -$
308 2 , $p = 0.045$). Similarly, arterial whole blood (C_b) and plasma (C_p) [¹¹C]PBR28 radioactivity
309 were significantly affected by IFN- α administration, compared to baseline conditions, with a

310 pattern indicating a reduction in the ligand available to bind to TSPO in the brain. Peak
311 activities and area under the curve (AUC) for both Cp and Cb TACs significantly increased
312 in the second scan, with relative differences of $30\pm 13\%$ for peak Cp (paired t-test $t_6=-2.63$,
313 $p=0.04$), $25\pm 4\%$ for AUC Cp (paired t-test $t_6=-5.11$, $p=0.002$), $14\pm 8\%$ for peak Cb (paired
314 t-test $t_6=-1.91$, $p=0.11$) and $34\pm 6\%$ for AUC Cb (paired t-test $t_6=-6.23$ $p=0.004$). Moreover, a
315 positive correlation was found between the peripheral plasma binding (1-fp) and both AUC
316 Cp (Pearson's $r=0.61$, $p=0.02$) and AUC Cb (Pearson's $r=0.64$, $p=0.01$) (Fig. 2B). These
317 associations were consistent with increased retention of the ligand in plasma to the
318 increased peripheral inflammatory proteins induced by IFN- α .

319
320 Considering the increased plasma binding of the ligand resulting from arterial blood
321 analyses, we corrected results for fp. Interestingly, after this correction, Vt paired t-test
322 between the 2 scans dramatically changed and was no longer significant, with four subjects
323 showing an increase in Vt (ranging from 3% to 198%) and three subjects showing a
324 decrease (ranging from -52% to -9%) (Fig. 2C, lower part), averaging $23\pm 31\%$ ($t=0.1$,
325 $p=0.91$). Similar results were present when analyzing specific ROIs (Fig. 2C, upper part).

326
327 Results did not change after we repeated all the analyses using the endothelial model
328 2TCM-1K, again showing a significant decrease using the unadjusted mean whole
329 brain $\% \Delta Vt$ ($-28\pm 19\%$, $t=-3.06$, $p=0.02$) and no differences in $\% \Delta Vt$ after fp correction
330 ($7\pm 54\%$, $t=0.59$, $p=0.57$) (Fig. 2A, 2B and 2C).

331
332 **FIGURE 2 around here**

333
334 *IFN- α increases peripheral biomarkers of inflammation*

335

336 IFN- α administration resulted in significant changes in serum biomarkers at 4-24 hours after
337 the challenge. Compared with 1 hour before IFN- α , repeated measures ANOVA was
338 significant for hsCRP ($F_{1,2,7,1}=44.3$, $p<0.001$), IL-6 ($F_{4,24}=29.70$, $p<0.001$), IL-7 ($F_{4,24}=6.49$,
339 $p=0.001$), IL-8 ($F_{2,5,15,3}=9.11$, $p<0.001$), IL-10 ($F_{1,3,7,9}=64.62$, $p<0.001$), IFN- γ
340 ($F_{1,6,10,0}=32.27$, $p<0.001$), TNF- α ($F_{4,24}=21.10$, $p<0.001$) and VEGF-A ($F_{4,24}=7.71$, $p<0.001$),
341 with significant increases (using LSD pairways comparisons) at both 4 and 6 hours for all
342 biomarkers, except hsCRP and IL-8 which increased at 24 hours only, IL-7 which increased
343 at 6 hours only, and VEGF-A which decreased at 24 hours (Fig. 3). Of note is also that
344 TNF- α was still increased at 24 hours. Kynurenine/Tryptophan (K/T) ratio also showed an
345 increase at 24 hours, but this did not reach statistical significance (86 ± 59.5 folds,
346 $F_{4,20}=1.94$, $p=0.1$) (Fig. 3). S100B protein did not change significantly (change at 24 hours:
347 $35\pm 60\%$, $F_{1,1,6,7}=3.4$, $p=0.1$).

348

349 Values of hsCRP measured at the time of the baseline and post-interferon PET scan
350 correlated with the ligand protein binding (1-fp) (Pearson's $r=0.57$, $p=0.03$) and were
351 inversely associated with K1 values estimates (Pearson's $r=-0.75$, $p=0.002$), indicating that
352 higher peripheral inflammation was associated with increased binding of the ligand to
353 plasma protein and decreased availability of the ligand for entry into the brain.

354

355 **FIGURE 3 around here**

356

357 *IFN- α induces transient mood changes and sickness symptoms*

358

359 We found increased sickness symptoms at 4-6 hours after the challenge (Fig. 4), as shown
360 by an increase in POMS-2 Total Mood Disturbance (TMD) ($F_{4,24}=4.6$, $p=0.006$), POMS-2
361 Confusion-bewilderment ($F_{4,24}=3.12$, $p=0.03$) and POMS-2 Fatigue-Inertia ($F_{1,2,7,2}=7.71$,
362 $p=0.02$) at 6 hours, and a reduction in POMS-2 Vigor-Activity ($F_{4,24}=5.86$, $p=0.02$) and
363 POMS-2 Friendliness ($F_{4,24}=3.80$, $p=0.02$) at 4 hours. Finally, the STAI-S scores peaked at
364 4 hours after IFN- α ($F_{4,24}=2.94$, $p=0.04$). Delta hsCRP (at 24 hours) was positively
365 correlated with delta POMS TMD score (at 6 hours) (Pearson's $r=0.88$, $p=0.009$).

366

367 **FIGURE 4 around here**

368

369 *IFN- α increases body temperature, blood pressure and heart rate*

370

371 Vital signs were closely monitored after IFN- α administration. From 1 hour before the
372 injection to 8 hours after, we detected significant increases in body temperature (+1.1 C,
373 from 36,3 C to 37,4 C, $t=-6.10$, $p=0.001$) and heart rate (+24 bpm, from 65 bpm to 89 bpm,
374 $t=-3.1$, $p=0.02$). Average but not statistically significant increases were found also in systolic
375 blood pressure (+16 mmHg, from 123 mmHg to 139 mmHg) and diastolic blood pressure
376 (+3 mmHg, from 63 mmHg to 66 mmHg).

377

378 **Discussion**

379

380

381 Here we investigate the association between peripheral and central inflammation in healthy
382 humans, using the immune challenge IFN- α . We show that IFN- α induces peripheral
383 inflammation that is comparable, and sometimes more intense, than that described in
384 depression, in association with acute mood changes. However, we cannot measure a

385 neuroinflammatory response with TSPO-PET imaging. Our thorough methodology
386 addresses all limitations affecting second generation high affinity tracers: we only select
387 high-affinity binders (HABs); we use both 2TCM and 2TCMK1 models to correct for
388 endothelial binding; and we normalize results for fp, that is, for the amount of ligand that is
389 able to enter the brain because it is free from binding to plasma proteins.

390

391 Overall, this study confirms that brain TSPO binding is strongly affected by the free-plasma
392 fraction artefact (32). The evidence that V_t changes are mainly explained by blood flow (K_1)
393 changes, and that the initial V_t decrease disappears after fp correction, indicates that the
394 signal differences between the two PET scans are mainly driven by changes in the
395 availability of free ligand in the plasma after the immune challenge. This is further
396 supported by the positive correlation between inflammation (hsCRP levels) and ligand
397 protein binding, and the negative correlation between hsCRP levels and K_1 . Our data thus
398 support the notion that peripheral inflammation, here occurring with the IFN- α injection,
399 induces an increase in the ligand's peripheral plasma binding and thus results in a lower
400 proportion of ligand available for TSPO binding in the brain. This important methodological
401 limitation suggests that the pathophysiological implications of altered brain TSPO-PET
402 signal are difficult to interpret, thus limiting its usefulness as a sensitive marker of
403 neuroinflammation and microglial activation. Of course, our findings are in apparent
404 contrast with the aforementioned studies which found increased brain TSPO-PET signal in
405 healthy humans after LPS injection, or in patients with depression, a condition associated
406 with increased inflammation. However, many mechanisms can explain this potential
407 discrepancy.

408

409 In the aforementioned study (23), LPS administration in eight healthy males induced much
410 stronger and faster peripheral pro-inflammatory responses compared with IFN- α in our
411 study, partly because LPS acts immediately on toll-like receptors that directly activate the
412 NK-FB pathway (14). IFN- α , instead, acts through several intermediate steps, including the
413 Jack/STAT/ISGF3 pathway (61), with the NK-FB pathway as an alternative route of action
414 (62). For example, IL-6 levels were approximately 100 pg/ml at 4 hours in the LPS study
415 (having reached an average of 200 pg/ml at previous time-points), while IL-6 levels average
416 around 6 pg/ml at 4 hours in our study. Consistent with this, the LPS in that study induced
417 much stronger physiological responses compared with IFN- α in our study, that is, twice the
418 increase in body temperature, and approximately +50% in the increase in heart rate.
419 Moreover, these changes happened already at 3 hours from the challenge, showing a
420 quicker mechanism of action compared with IFN- α . Finally, and most relevant for the
421 potential discrepancy with our findings, the LPS study did not apply the fp correction, so we
422 have no information on the relationship between acute LPS-induced inflammation, free
423 ligand in the plasma, and brain TSPO signal. Incidentally, this same limitation also applies
424 to the two studies using LPS in non-human primates (21, 22).

425

426 The second finding in apparent contrast with our results is the presence of increased TSPO
427 binding in patients with depression, as shown by some of the studies conducted so far.
428 However, it is of note that the two studies which used [^{11}C]PBR28 *and* corrected for fp
429 effect, like we do, found no difference (6), or a borderline-significant increase, in TSPO-PET
430 signal (11). The other studies that found increased TSPO-PET signal (7-10, 18) used
431 different, first and second generation radioligands, and did not correct for fp, and so they
432 did not take into consideration the ligand binding to plasma proteins. Moreover, of the
433 studies reporting an increased TSPO-PET signal, only two examined depressed patients

434 with increased inflammation (8, 10), and TSPO-PET signal in depressed patients did *not*
435 correlate with peripheral inflammation.

436

437 It is interesting to note that the levels of peripheral inflammation in our study do indeed
438 resemble those present in patients with major depression. For example, the Hedges effect
439 size of IL-6 and TNF- α differences from baseline to 24 hours after IFN- α are 0.48 and 0.66,
440 respectively, which are very close to the difference between controls and patients with
441 depression for these two cytokines, as shown by Hedges $g=0.62$ and 0.68 , respectively
442 (63). Values of hsCRP at 24 hours are higher in our study compared with average
443 depressed patients' values, as we obtain a mean of around 10 mg/L and Hedges' $g=1.69$
444 compared with baseline, vs values in most depressed patients between 1 and 3 mg/L (13)
445 and Cohen's $d=0.47$ for the difference between controls and depressed patients (64).
446 However, values reached in our study still have clinical relevance for mental health, as one
447 previous study has found that CRP levels above 10 mg/L are associated with a high risk of
448 developing future depression (65). Thus, the immune challenge with acute IFN- α can be
449 used to examine the neural and immunological regulatory response to an immune
450 perturbation that is within the same magnitude of that described in depression, as opposed
451 to, for example, the much more intense activation of inflammatory processes induced by
452 LPS in the aforementioned study (23). Further discussion of our immune findings, including
453 the reduction of VEGF-A, is in the Supplementary Material.

454

455 Of course, brain TSPO-PET signal is markedly upregulated in clinical conditions that have
456 neuroinflammation at their core, such as Huntington's disease or multiple sclerosis. Indeed,
457 positive correlations between levels of pro-inflammatory cytokines and brain TSPO-PET
458 signal have been found in neurological conditions associated with genuine

459 neuroinflammatory processes (66), but not in studies of psychiatric patients (67, 68). Thus,
460 beyond the different technical approaches in the analyses of the PET data, the variability in
461 the results of TSPO-PET studies in psychiatric patients (or in studies that, as ours, mimic
462 the levels of peripheral inflammation described in psychiatric patients), may simply reflect a
463 true lack of microglial activation. Indeed, Notter and colleagues (68) have recently
464 highlighted that the brain expression of inflammation-related genes, the microglial
465 phenotypes, the presence of reactive gliosis, and the levels of cerebrospinal fluid (CSF)
466 cytokines, are all very different in true neuroimmunological disorders, such as multiple
467 sclerosis, compared with psychiatric disorders. Thus, PET radiotracers targeting alternative
468 markers of immune response might be needed to capture inflammatory processes in the
469 brains of patients with psychiatric disorders (69), together with CSF analyses, as recently
470 done by Felger and colleagues (70) and other studies in depressed patients (4). Moreover,
471 TSPO signal can be driven by factors other than microglial activation (71), such as
472 recruitment of peripheral monocytes into the parenchyma, adherence of circulating
473 leucocytes to the vascular endothelium, and the expression of TSPO in various brain cells,
474 including microglia, astrocytes, vascular endothelial cells and neurons. Unfortunately, the
475 lack of cellular specificity is often neglected when interpreting PET studies, as well the
476 potential changes in blood-brain barrier permeability and the need to correct for the
477 endothelial component of TSPO signal (as we do in our study). Nevertheless, as our
478 challenge is acute, we cannot exclude the possibility that some depressed patients do have
479 increased brain TSPO-PET signal because of microglial activation, as a consequence of
480 increased inflammation lasting months or even years before the study, rather than just 24
481 hours. In fact, long-lasting inflammation in depression may in fact be driven either by early
482 risk factors, such as childhood maltreatment or antenatal depression (72-74), or present
483 during previous relapses or exacerbations, even if not measurable on the day of the scan.

484

485

486 This study has some limitations. First, it is possible that the timing of the second PET scan
487 might not have been ideal to detect neuroinflammation. Although we had based our
488 decision to do the second scan at 24 hours on pre-clinical studies (33), we find that
489 significant sickness symptoms were present at around 4-6 hours after the challenge,
490 together with the peak in IL-6, IL-10 and IFN- γ , so we cannot exclude that an increased
491 brain TSPO binding could have been measured at that timepoint. It is also possible that a
492 regulatory anti-inflammatory response could have started at 24 hours, and this could have
493 confounded the results. However, some other inflammatory markers relevant to depression
494 were either increased only at 24 hours (hsCRP, IL-8) or increased at all time-points,
495 including 24 hours (TNF- α), indicating that systemic inflammatory processes were still
496 present at the time of the second scan. Our research was also limited by the small sample
497 size. However, PET studies are extremely invasive, challenging and expensive, and studies
498 with two repeated PET scans at such a short distance tend to have numbers in the range of
499 6-8 subjects, like in the aforementioned study in healthy humans with LPS which had 8
500 subjects (23).

501

502 **Conclusion**

503

504 To our knowledge, this is the first study assessing central inflammatory responses to IFN- α
505 in healthy humans by using PET together with an assessment of peripheral inflammatory
506 biomarkers. While the ability of IFN- α to induce acute inflammatory responses and mood
507 changes highlights its potential as an immune model of depression for future studies in
508 healthy humans, we find no evidence of a putative neuroinflammatory response, and we

509 unequivocally demonstrate that brain TSPO-PET signal measurement is confounded by the
510 inflammation-induced changes in [¹¹C]PBR28 free ligand in the plasma. In conclusion, there
511 is an urgent call for new targets of microglial activation that could also better clarify the role
512 of TSPO in measuring neuroinflammation, especially if coupled with CSF analysis.

513

514

515 **Acknowledgments**

516 This study represents independent research supported by the NIHR Biomedical Research
517 Centre at South London and Maudsley NHS Foundation Trust and King's College London,
518 and the National Institute for Health Research NIHR / Wellcome King's Clinical Research
519 Facility. The views expressed are those of the author(s) and not necessarily those of the
520 NHS, the NIHR or the Department of Health and Social Care. All IFN- α visits took place at
521 the Clinical Research Facility of King's College Hospital. The team of nurses, in particular
522 the Lead Experimental Research Nurse, Noah Yogo, has to be thanked for providing their
523 valuable expertise to the study. This study was also supported by Janssen Pharmaceutical
524 Companies of Johnson&Johnson. [¹¹C]PBR28 synthesis, as well as all PET scans, were
525 conducted at Invicro (Imperial college London), whose staff provided an excellent technical
526 contribution. We also thank Dr M. Tonietto for the plasma protein binding analysis.

527

528

529 **Conflicts of Interest**

530 Professor Pariante, Professor Turkheimer and Dr Mondelli have received research funding
531 from Janssen Pharmaceutical NV/Janssen Pharmaceutical, Companies of
532 Johnson&Johnson, partly also contributing to this study.

533 Supplementary information is available at TP's website.

534

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760 **Tables and Figures Captions**

761

762 **Table 1** Sociodemographic data at Screening Visit

763

764 **Fig.1** Study design

765

766 **Fig. 2** IFN- α administration effect on [11 C]PBR28 binding (V_t) from baseline in healthy
767 control subjects (n = 7) before (A) and after (C) fp correction. Results are showed as
768 regional percent increase in V_t (ΔV_t) averaged across subjects (top images error bars are
769 SEM) and V_t change for each subject averaged across regions (bottom images). (B) Peak
770 activities and area under the curve (AUC) for both plasma (C_p) and whole blood (C_b)
771 showed a significant increase in the second scan and positively correlated with plasma
772 protein binding.

773

774 **Fig. 3** Peripheral response: peripheral cytokines levels increased after 4-6 hours after the
775 IFN- α challenge; hsCrp levels raised at 24 hours after IFN- α ; K/T ratio increased at 24
776 hours after IFN- α . Data are presented as mean and standard errors of the mean.

777

778 **Fig. 4** IFN- α administration effect on clinical measures over time. POMS-2 and STAI-S
779 scores increased significantly between 4 and 6 hours after the challenge. Data are
780 presented as mean and standard errors of the mean.

781

782

783

TABLE 1

Subject	Age (years)	Ethnicity	BMI (kg/m²)
1	28	Black-African	20.38
2	25	Black-African	23.12
3	33	Asian-Filippino	24.54
4	43	Black-African	24.68
5	29	White-British	23.62
6	26	Black-Caribbean	25.62
7	25	Mixed	22.24
Mean±SD	29.85±6.44	-	23.46±1.75

FIGURE 1

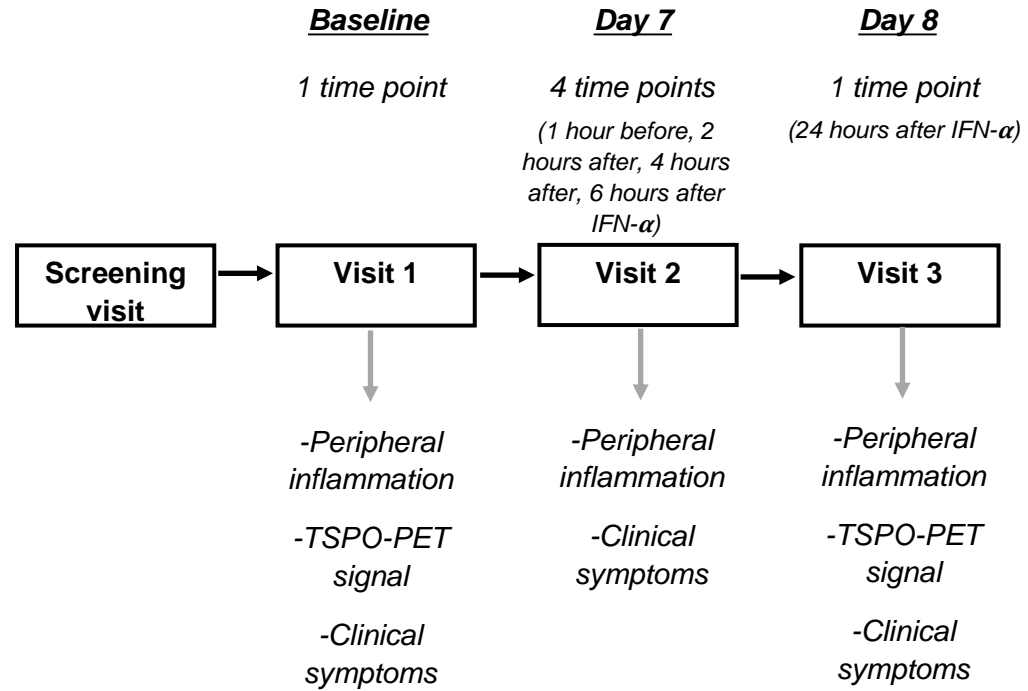


FIGURE 2

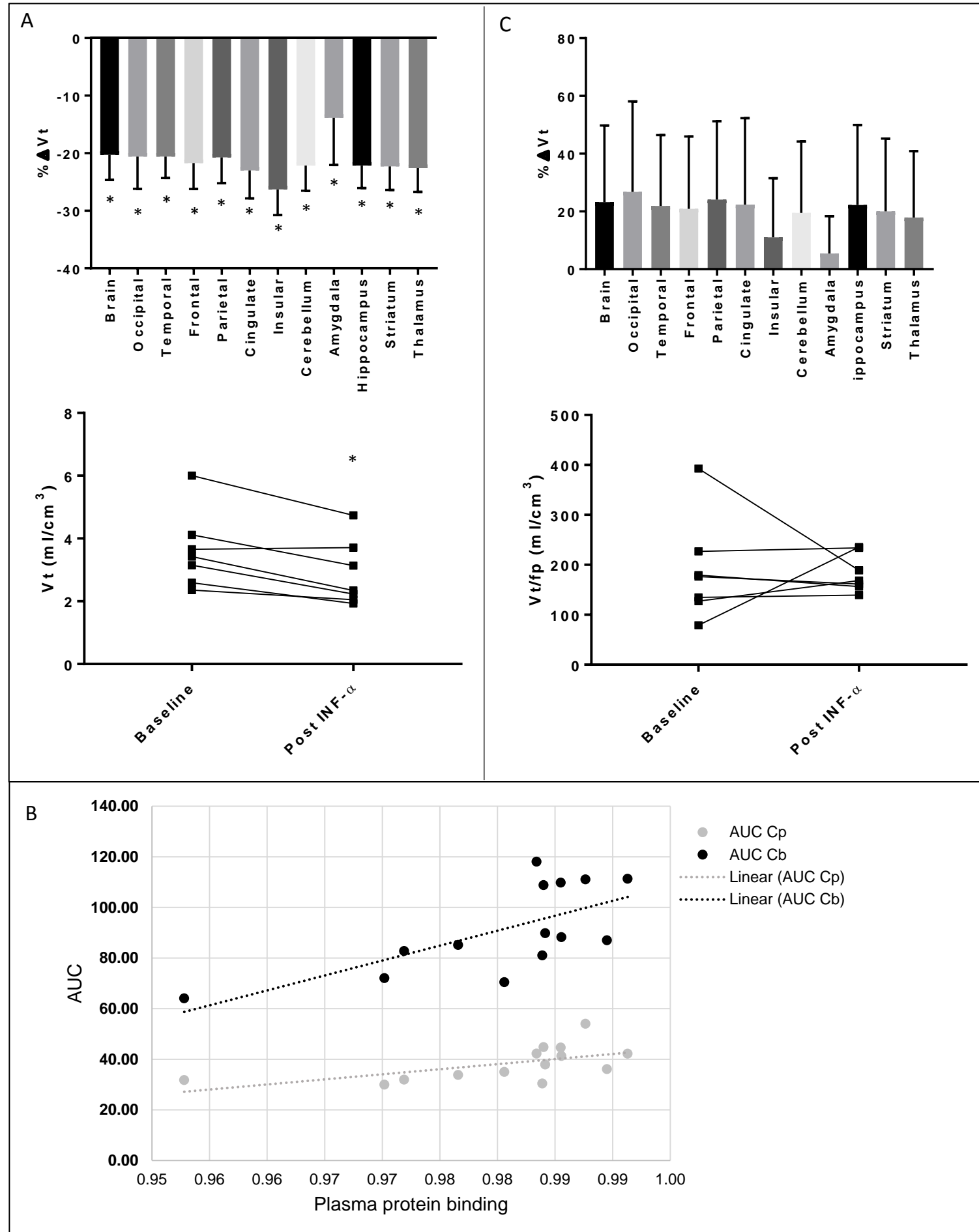


FIGURE 3

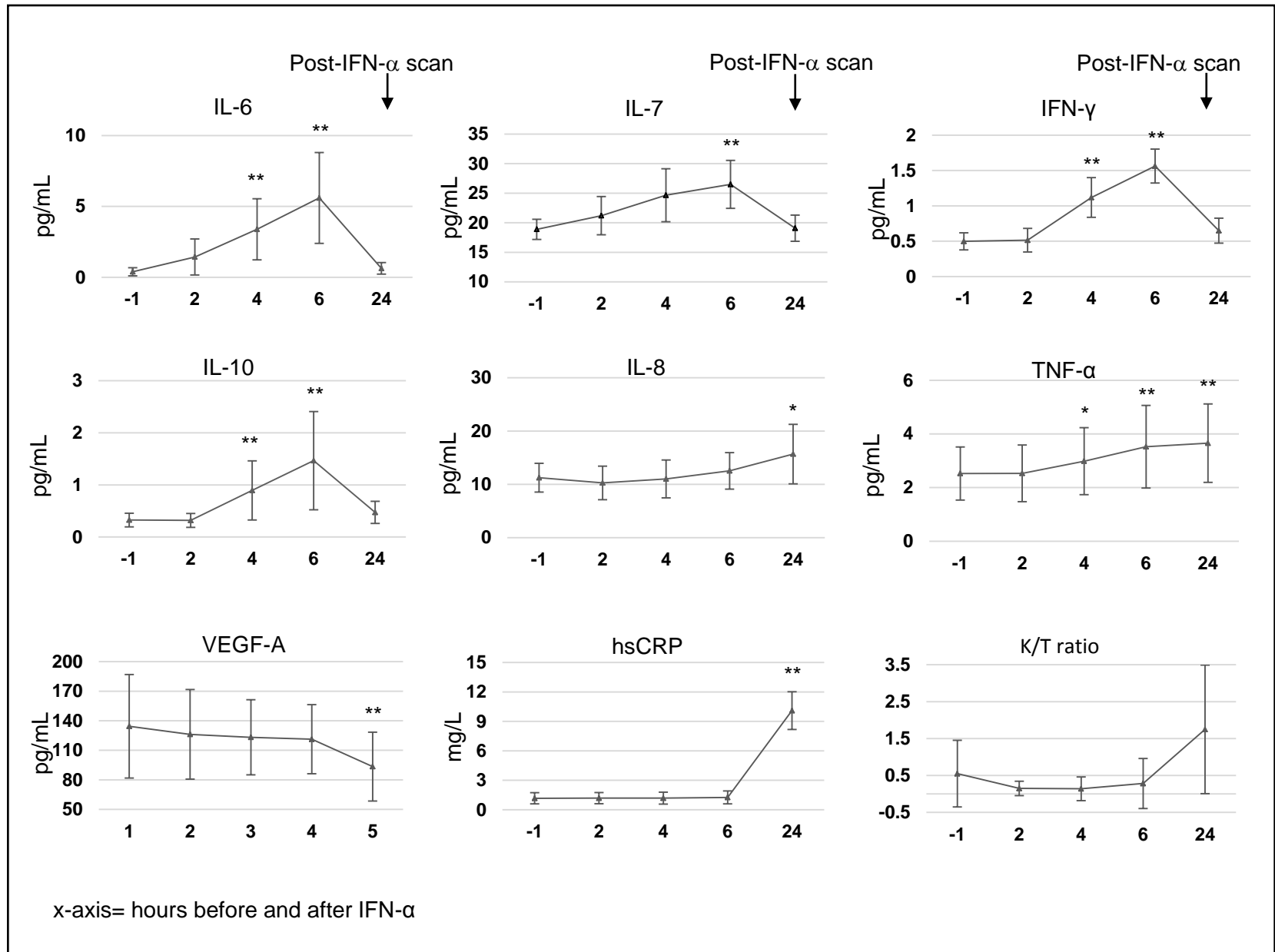


FIGURE 4

