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# CAMANet: Class Activation Map Guided Attention Network for Radiology Report Generation

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# A B S T R A C T

Radiology report generation (RRG) has gained increasing research attention because of its huge potential to mitigate medical resource shortages and aid the process of disease decision making by radiologists. Recent advancements in Radiology Report Generation (RRG) are largely driven by improving models' capabilities in encoding single-modal feature representations, while few studies explore explicitly the cross-modal alignment between image regions and words. Radiologists typically focus first on abnormal image regions before they compose the corresponding text descriptions, thus cross-modal alignment is of great importance to learn an abnormality-aware RRG model. Motivated by this, we propose a Class Activation Map guided Attention Network (CAMANet) which explicitly promotes cross-modal alignment by employing the aggregated class activation maps to supervise the cross-modal attention learning, and simultaneously enriches the discriminative information. Experimental results demonstrate that CAMANet outperforms previous SOTA methods on two commonly used RRG benchmarks.<sup>[1](#page-1-0)</sup> Chan Wang', Abbit Philosophy Analysis November 1, 2022 archives the Medical Internal I

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# 1. Introduction

Radiology report generation (RRG) aims to automatically describes radiology images, e.g., X-Ray and MRI, by human-like language. Generating a coherent report requires expertise from radiologists, who are however among the most in-demand physician specialists in most countries. Moreover, it can take at least 5 minutes to describe a radiology image even for a professional radiologist [\(Jing et al., 2018\)](#page-16-0). Consequently, there had been growing interest in automating RRG because of its huge potential to efficiently and effectively assist the diagnosis process.

RRG is a challenging task and with the availability of large-scale datasets and newly developed high-performance computer vision and language models, some valuable insights and improvements have been recently reported [\(Miura et al., 2021;](#page-16-1) [Nishino](#page-16-2) [et al., 2020;](#page-16-2) [Liu et al., 2019\)](#page-16-3). The performance however is still far from satisfactory for methods to be deployed in practice. This is

<span id="page-1-0"></span><sup>&</sup>lt;sup>1</sup>Our source code and trained models will be made available upon paper acceptance.

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<span id="page-2-0"></span>Fig. 1. A Chest X-Ray image with its report findings. The aligned visual and textual features are marked in the same color.

because, different from the traditional image captioning task which mostly requires generating 1 or 2 sentences, RRG requires 2-4 times *more* sentences to describe potentially abnormal regions in an image. Also, radiology reports tend to contain sentences with more sophisticated semantic relationships with their corresponding image regions, calling for a need for *more precise* cross-modal alignment, i.e., alignment between words and image regions. An example is shown in [Figure 1](#page-2-0) where the cross-modal alignments are marked in the same color. The problem is exacerbated as there exist data biases in commonly used datasets with significantly fewer radiology reports about X-ray images containing abnormal regions, making it hard for the RRG models to efficiently capture abnormal features which often exist only in small parts of pathological images. What is worse, even in pathological cases, most report statements may be associated with a description of normal findings, as shown in [Figure 1.](#page-2-0)

Previous approaches [\(Zhang et al., 2020;](#page-17-0) [Jing et al., 2018;](#page-16-0) [Chen et al., 2020,](#page-16-4) [2021\)](#page-16-5) often focus on improving the visual representation capability or better learning the semantic patterns by utilizing a learnable memory, while few studies explicitly explore representation learning with information about image abnormality detection and cross-modal alignment. To bridge this gap, we propose a Class Activation Map guided Attention Network (CAMANet) which distills the discriminative information into the encoder and explicitly improve cross-modal alignment by leveraging class activation maps [\(Zhou et al., 2016\)](#page-17-1).

This work makes four principal contributions:

- 1. A novel end-to-end class activation map guided attention model where the class-activation map is utilized to explicitly promote the cross-modal alignment and discriminative representation learning. To the best of our limited knowledge, CAMANet is the first work to leverage class activation maps in this way.
- 2. A Visual Discriminative Map (VDM) Generation module designed to derive the visual discriminative map from the class activation maps based on the pseudo labels from an automatic labeler.
- 3. A VDM Assisted Encoder which enriches the discriminative information by utilizing the self-attention mechanism and the VDM.
- 4. A visual-textual attention consistency module which considers the VDM as the ground truth to supervise the cross-modal attention learning in the decoder, so as to explicitly promote the cross-modal alignment.

Experimental results demonstrate that CAMANet outperforms the previous state-of-the-art methods on two widely-used benchmarks. We conduct ablation studies to further verify the effectiveness of each proposed individual component in CAMANet. Discussion and proposals are given to inspire future work.



<span id="page-3-0"></span>Fig. 2. The architecture of CAMANet: An image is fed into the Visual Extractor to obtain patch features which are then utilized to generate the VDM via the VDM Generation module. The proposed VDMAE leverages the VDM to derive a discriminative representation and enrich the discriminative information. Combined with the word embedding, the visual tokens are sent to the transformer to produce the report. After that, the VTAC module generates a TDM from the cross-modal attention scores and considers the VDM as the ground truth to supervise the cross-modal alignment learning.

#### 2. Related Work

#### *2.1. Image Captioning*

Image captioning, aiming to describe an image with human-like sentences, is considered as a high-level visual understanding problem taking advantage of both the techniques of computer vision and natural language processing. Because of the great success in the machine translation and language generation, recent state-of-the-art approaches [\(Pei et al., 2019;](#page-17-2) [Wang et al., 2020;](#page-17-3) [Liu et al.,](#page-16-6) [2018;](#page-16-6) [Lu et al., 2017;](#page-16-7) [You et al., 2016;](#page-17-4) [Rennie et al., 2017\)](#page-17-5) also follow an encoder-decoder architecture and have demonstrated a great improvement in some traditional image captioning benchmarks. In particular, the most successful models [\(Cornia et al., 2020;](#page-16-8) [Guo et al., 2020;](#page-16-9) [Pan et al., 2020;](#page-16-10) [Ji et al., 2021\)](#page-16-11) usually adopt the Transformer [\(Vaswani et al., 2017\)](#page-17-6) as their backbone due to its self-attention mechanism and impressive capability of modelling long-range dependency. However, these methods are tailored for traditional scene images, and not suitable for the radiology images with long sentence report and fine-grained, abnormal regions. Though several works [\(Krause et al., 2017;](#page-16-12) [Melas-Kyriazi et al., 2018\)](#page-16-13) have been developed to tackle the long text generation, they often fail in capturing specific medical observations and tend to generate normal descriptions, resulting in unsatisfactory performance.

# <span id="page-3-1"></span>*2.2. Radiology Report Generation*

Following on from the success in image captioning [\(Cornia et al., 2020;](#page-16-8) [Guo et al., 2020;](#page-16-9) [Pan et al., 2020;](#page-16-10) [Ji et al., 2021;](#page-16-11) [Pei](#page-17-2) [et al., 2019;](#page-17-2) [Wang et al., 2020;](#page-17-3) [Liu et al., 2018\)](#page-16-6), recent state-of-the-art (SOTA) RRG studies all adopt similar architectures: an encoder-decoder to generate the report combined with a convolutional neural network as the visual extractor. For example, [Jing](#page-16-0) [et al.](#page-16-0) [\(2018\)](#page-16-0) proposed a hierarchical LSTM model to mitigate the long sentence problem and developed a co-attention mechanism to localize abnormal regions. Other works have utilized disease topic information [\(Liu et al., 2019;](#page-16-3) [Zhang et al., 2020\)](#page-17-0) and obtain

better results. [Liu et al.](#page-16-14) [\(2021b\)](#page-16-14) extended these works by taking advantage of both the prior and posterior knowledge, i.e., knowledge from the similar images and a predefined topic bag for report generation. [Chen et al.](#page-16-4) [\(2020\)](#page-16-4) designed a relational memory and a memory-driven conditional layer normalization to better learn the report patterns.

The aforementioned studies often neglect the importance of the cross-modal alignment and the discriminative (disease-related) representation learning. As the only work we know exploring the cross-modal alignment in RRG, R2GenCMN [\(Chen et al., 2021\)](#page-16-5), designed a shared memory matrix, expected to be able to implicitly learn the cross-modal alignment. However, learning the crossmodal alignment in this way proves difficult since the model is only trained under the cross entropy loss for report generation without any other forms of supervision/guidance for the cross-modal alignment learning. To address these problems, we propose a visual-textual attention consistency module to explicitly promote the cross-modal alignment learning by formulating a task that forces the visual and textual modalities to focus on the same image regions. In addition, we develop a VDM assisted encoder to enrich the discriminative information.

There are a few works [\(Zhou et al., 2020;](#page-17-7) [Chen et al., 2018\)](#page-16-15) exploring the image-word matching in scene images, which are similar to the cross-modal alignment. However, these methods normally require a well pre-trained fully-supervised detector, e.g Fast RCNN [\(Girshick, 2015\)](#page-16-16) and Faster RCNN [\(Ren et al., 2015\)](#page-17-8) trained on ground truth labels to detect generate the object proposals offline. In addition, they have the valuable bounding box annotation and utilize it to form the mapping supervision. However, there is no large dataset on radiology report generation task containing the costly and valuable ground truth labels to train an accurate detector and form the extra supervision. As a result, they are unsuitable for radiology report generation tasks, and we need to integrate and train the visual extractor in the whole architecture and discover an alternative way to perform the cross-modal alignment. Another significant difference between our work and [\(Zhou et al., 2020\)](#page-17-7) is that the supervision of [\(Zhou et al., 2020\)](#page-17-7) is applied on each word-region pair thus making it difficult to learn, while our method improves the cross-modal alignment by ensuring the consistency between the block-level, derived visual and textual discriminative maps.

#### *2.3. Class Activation Maps*

Proposed by [Zhou et al.](#page-17-1) [\(2016\)](#page-17-1), a class activation map (CAM) was first used for weakly supervised object detection [\(Jiang et al.,](#page-16-17) [2021;](#page-16-17) [Bae et al., 2020;](#page-16-18) [Xie et al., 2021\)](#page-17-9), aiming to localize the objects with only image-level annotations. CAMs can identify the discriminative regions in an image by utilizing the *global average pooling layer* (GAP). Consequently, this technique is adopted in some weakly supervised semantic segmentation methods [\(Ru et al., 2022;](#page-17-10) [Sun et al., 2021;](#page-17-11) [Chen et al., 2022\)](#page-16-19) to generate the pseudo labels and provides performance gains. Different from these works, here we use a CAM to enhance the discriminative representation capability and the cross-modal alignment. We have not seen CAMs being leveraged in this way for the RRG task.

#### 3. Method

Before detailing our method, in Section [3.1](#page-4-0) we give some background of RRG including the problem formulation and the general architecture. In Section [3.2,](#page-5-0) we elaborate each proposed component of CAMANet. The objective function is finally described in Section [3.3.](#page-8-0) An overview of the CAMANet architecture is illustrated in [Figure 2.](#page-3-0)

#### <span id="page-4-0"></span>*3.1. Background*

Given a radiology image *I*, such as a chest X-Ray image, the purpose of RRG is to generate the coherent findings (report) **R** from *I*. Recent state-of-the-art methods often adopt an encoder-decoder framework to generate the report. In particular, a visual extractor, e.g. ResNet101 [\(He et al., 2016\)](#page-16-20) or DenseNet121 [\(Huang et al., 2017\)](#page-16-21), is first employed to extract visual features  $v^i \in \mathbb{R}^{H \times W \times C}$ 

Lung Opacity	Cardiomegaly	No Finding		
Lung Lesion	Consolidation	Edema		
Pneumothorax	Pneumonia	Atelectasis		
Pleural Effusion	Pleural Other	Fracture		
<b>Support Devices</b>	<b>Enlarged Cardiomediastinum</b>			

<span id="page-5-1"></span>Table 1. The 14 categories predefined and output by the automatic labeler.

which are then flattened to a sequence of visual tokens  $v^s \in \mathbb{R}^{HW \times C}$ . *H*, *W*, *C* are the height, width and the number of channels respectively. This process is formulated as:

<span id="page-5-2"></span>
$$
\{v_1^s, v_2^s, ..., v_k^s, ..., v_{N^s-1}^s, v_{N^s}^s\} = f_i(\mathbf{I}),
$$
\n(1)

where  $v_k^s$  denotes the patch feature in the  $k^{th}$  position in  $v^s$ , and  $N^s = H \times W$ .  $f_i$  is the visual feature extractor.

These visual tokens are then fed into the transformer based encoder-decoder to generate a report *R*. Specifically, at time step *T*, the encoder maps the visual tokens into an intermediate representations  $I^i \in \mathbb{R}^{1 \times D}$ . An embedding layer is applied to obtain the word embedding  $I^r \in \mathbb{R}^{1 \times D}$  of each word *w* in the report *R*. *D* is the number of dimensions of hidden states. After this, the decoder takes these two sequence features as source inputs and predicts the current output (word). In general, we express the encoding and decoding processes as:

<span id="page-5-3"></span>
$$
\{l_1^i, l_2^i, ..., l_{N^s}^i\} = f_{en}(v_1^s, v_2^s, ..., v_{N^s}^s),
$$
\n(2)

$$
\{l_1^r, l_2^r, \dots, l_{T-1}^r\} = f_{em}(w_1, w_2, \dots, w_{T-1}),\tag{3}
$$

$$
p_T = f_{de}(l_1^i, l_2^i, ..., l_N^s; l_1^r, l_2^r, ..., l_{T-1}^r),
$$
\n(4)

Where the  $f_{en}$ ,  $f_{em}$  and  $f_{de}$  denotes the encoder, embedding layer and the decoder respectively.  $p_T$  is the word prediction at time step *T*.

The core of the encoder and decoder is the attention mechanism *Attn*, [Vaswani et al.](#page-17-6) [\(2017\)](#page-17-6), expressed as,

$$
Attn(Q, K, V) = softmax(\frac{QK^{T}}{\sqrt{d}}),
$$
\n(5)

$$
Q = W_q \cdot q, K = W_k \cdot k, V = W_v \cdot v,
$$
\n<sup>(6)</sup>

where  $W_a$ ,  $W_k$  and  $W_v$  are weights and  $q$ ,  $k$  and  $\nu$  refer to the query, key and value respectively. *d* is the number of dimensions of the hidden states. Note that different from the self-attention layer in other modules where the query, key and value are the same, e.g, visual token or textual token sequence, the second attention layer in the decoder takes the textual tokens as the query and the visual tokens as the key/value. To differentiate it from a typical attention layer, we name it as the *cross-modal attention* in this paper. We refer interested readers to [\(Vaswani et al., 2017\)](#page-17-6) to understand details of the computation of self-attention in Transformers. We next present the details of the proposed CAMANet.

#### <span id="page-5-0"></span>*3.2. CAMANet*

Learning the cross-modal alignment and discriminative representation is challenging but essential for RRG. To achieve this, CAMANet uses a Visual Discriminative Map Assisted Encoder (VDMAE) and a Visual-Textual Attention Consistency (VTAC) module which take advantage of the class activation map (CAM) [\(Zhou et al., 2016\)](#page-17-1) technique.

#### *3.2.1. Visual Discriminative Map Generation*

The first step is to generate a visual discriminative map indicating the discriminative regions in an image. This discriminative map is then used in the VDM Assisted Encoder (VDMAE) and the Visual-Textual Attention Consistency (VTAC) modules to enable the discriminative representation learning and cross-modal alignment.

We propose to leverage the class activation map (CAM) technique to localize discriminative regions. CAM requires the image category labels to form a classification task, so as to obtain the patch contributions (importance) to each category. The category labels are often unavailable for RRG datasets because of the time and expense required to create them. To overcome this problem in CAMANet, we utilize CheXbert [\(Smit et al., 2020\)](#page-17-12), an automatic labeller, to generate a pseudo label *y* for each image. We can form a multi-label classification task given that *y* is a multi-hot vector encoding the presence of 14 common observations in Chest X-ray images is given in [Table 1.](#page-5-1) As shown in the lower right red box in [Figure 2,](#page-3-0) a classification head is added, taking the extracted visual tokens from the visual extractor as input, to predict the presence  $\tilde{y}_i \in 0, 1$  for  $i^{th}$  disease formulated as:

$$
v_g = \frac{1}{N^s} \sum_{j=1}^{N^s} v_j^s,
$$
\n(7)

$$
\{\widetilde{y}_1, \widetilde{y}_2, ..., \widetilde{y}_{N^c}\} = \Phi(S \text{ of } \max(\mathbf{W}_c \cdot \mathbf{v}_g)),\tag{8}
$$

$$
\Phi(o) = \begin{cases}\n0 & \text{if } o \le 0.5, \\
1 & \text{if } o > 0.5,\n\end{cases}
$$
\n(9)

where  $v_g$  and  $W_c$  denote the global visual feature and weights of the classification head.  $N^c$  is the number of disease categories.

After the forward process of the visual extractor, we can obtain the class activation map  $m^i = \{m_1^i, m_2^i, ..., m_{N^s}^i\}$  for  $i^{th}$  category with  $\tilde{y}_i = 1$ . Remember that the classification is for the multi-label scenario, hence each sample may show the presence of multiple observations. To this end, we aggregate the class activation maps for all the categories present and generate a visual discriminative map  $d^v$  to target important regions. In particular, we first use the ReLU activation function to zero out negative contributions. Min-max normalization is then applied to each class activation map. [Equation 10](#page-6-0) formulates this process on the class activation map of *i th* category *m<sup>i</sup>* :

<span id="page-6-0"></span>
$$
\widetilde{m}_j^i = \frac{\sigma(m_j^i) - \min(\sigma(m^i))}{\sigma(\max(m^i)) - \sigma(\min(m^i))},\tag{10}
$$

where  $\widetilde{m}_j^i$  is the normalized contribution/importance of  $j^{th}$  patch for  $i^{th}$  category and  $\sigma$  denotes the ReLu activation function. Then, the final visual discriminative map  $d^v \in \mathbb{R}^{1 \times N^s}$  is obtained via maximum pooling over all the class activation maps:

$$
d^{\nu} = MaxPool(\{m^k|\widetilde{y}_k=1\}).
$$
\n(11)

Note that though we utilize the class activation map technique to generate the visual discriminative map, any weakly supervised techniques producing patch-level scores could be applied here. As discussed in [subsection 2.2](#page-3-1) weakly supervised detection techniques, e.g., Region Of Interest (ROI) based weekly supervised models will generate region-level scores and require a well-trained detector, so is unsuitable to RRG.

#### <span id="page-6-1"></span>*3.2.2. VDM Assisted Encoder*

Since the dataset is dominated by normal samples, e.g., normal images and descriptions, the RRG model struggles to capture abnormal information and describe abnormal regions. To mitigate this problem, we propose a visual discriminative map (VDM) assisted encoder, the VDMAE, to enrich the discriminative information. This is achieved by learning a discriminative representation in terms of the VDM  $d^v$ , which is distilled into the encoder. We show this procedure by the green rectangle in [Figure 2.](#page-3-0) Specifically,

the discriminative representation  $r \in \mathbb{R}^{1 \times C}$  is obtained by matrix multiplication between the visual discriminative map  $d^v \in \mathbb{R}^{1 \times N^s}$ and the image patch features,

$$
r = d^{\nu} \otimes \nu^{s}, \tag{12}
$$

where  $v^s \in \mathbb{R}^{N^s \times C}$  is the extracted visual token sequence obtained by [Equation 1](#page-5-2) and ⊗ denotes matrix multiplication. A normalization layer is further added to stabilize the distribution:

$$
r' = LayerNorm(r). \tag{13}
$$

After obtaining the discriminative representation, we add it as an extra visual token as input to the encoder and leverage the power of an attention mechanism to gradually incorporate the VDM features for representation learning. Then [Equation 2](#page-5-3) becomes:

$$
\{\mathbf{r}^{\star}, l_1^i, ..., l_{N^i}^i\} = f_{en}(\mathbf{r}^{'}, v_1^s, ..., v_{N^i}^s). \tag{14}
$$

Through the self-attention mechanism in the encoder, other visual tokens can fully interact with this to learn the useful discriminative information. Note that the encoded discriminative representation  $r^*$  is detached in the decoder for the sake of better cross-modal alignment in the visual-textual attention consistency module. We elaborate this further in the next section.

#### *3.2.3. Visual-Textual Attention Consistency*

Cross-modal alignment is essential to learn a coherent and disease-aware model. Previous work learns the alignment implicitly either by a cross-modal attention in the decoder or through a shared memory. However, such strategies are less efficient considering the severe data bias problem and more sophisticated sentence discourse relations in radiology reports. We therefore design a Visual-Textual Attention Consistency (VTAC) module to explicitly learn the cross-modal alignment using the visual discriminative map  $d<sup>v</sup>$ as the ground truth to supervise the cross-modal attention learning in the decoder, as demonstrated in the upper right blue rectangular in [Figure 2.](#page-3-0) The intuition behind this is that when generating a report, the language model should attend to the same regions, e.g., those discriminative regions, as the visual classifier which aims to detect abnormal regions.

Nonetheless, each word in the report has its own attention to the image in the cross-modal attention. This raises a question of how to utilize a single discriminative map to supervise multiple attentions from different words. To deal with this problem, we also form a textual discriminative map  $d^t$  by aggregating the attentions from *important* words. Then the problem turns to how best to select them and aggregate their attention maps.

One simple way to achieve this is the Term Frequency-Inverse Document Frequency (TF-IDF) [\(Ramos et al., 2003\)](#page-17-13) score, which however, is not suitable for radiology report corpus as the important words, e.g., medical name entities, in medical domain normally have low TF-IDF scores. For instance, most reports have the words "lung" and "heart" which leads to a low inverse document frequency value, and the frequency of theses words in one report normally just one or two. Therefore, the TF-IDF value of these words is small. For example, the IDF value for "heart" on IU-Xray dataset is 1.51 which is similar to the word "is" (IDF 1.43), "are" (IDF 1.33) and "and" (IDF 1.52). Nonetheless, these medical terms are important and should be selected when performing the cross-modal alignment.

To this end, we propose to use the encoded visual discriminative representation *r* ? which contains rich visual discriminative information, to select the attended words. More concretely, we expect that the embeddings of important words should have higher similarity to the visual discriminative representation in the latent space. Specifically, we first compute the cosine similarities between the embedding of each word and the visual discriminative representation via:

$$
s_j = \frac{l_j^r \cdot r^\star}{|l_j^r||r^\star|},\tag{15}
$$

where  $s_j$  denotes the similarity between  $j<sup>th</sup>$  word and the discriminative representative and  $\cdot$  is the dot product operation.

Then, the top *k*% words with the higher similarities are selected to generate a textual discriminative map. Given the cross-model attention scores  $A = \{a^1, a^2, ..., a^{\gamma}\}\$  of important words from the cross-modal attention layer in the final decoder, the generation of the *textual* discriminative map  $d^t \in \mathbb{R}^{1 \times N^s}$  is derived via [Equation 16](#page-8-1) and [Equation 17,](#page-8-2) which is similar to the generation of the *visual* discriminative map,

<span id="page-8-2"></span><span id="page-8-1"></span>
$$
\widetilde{a_j^i} = \frac{\sigma(a_j^i) - \min(\sigma(a^i))}{\sigma(\max(a^i)) - \sigma(\min(a^i))}
$$
(16)

$$
\begin{aligned}\n\alpha_j &= \sigma(\max(\boldsymbol{a}^i)) - \sigma(\min(\boldsymbol{a}^i)) \\
\boldsymbol{d}^t &= MaxPool([\boldsymbol{\widetilde{a}}^1, \boldsymbol{\widetilde{a}}^2, ..., \boldsymbol{\widetilde{a}}^{\gamma}]),\n\end{aligned}\n\tag{17}
$$

where  $\tilde{a}_j^i$  is the normalized attention score of  $i^{th}$  word for  $j^{th}$  image region. N<sup>r</sup> denotes the number of words in the report.  $\gamma = \lceil k \times N^r \rceil$ is the number of selected words to generate the textual discriminative map.

However, since [Equation 17](#page-8-2) does not consider the relative importance of the selected words, we utilize the calculated similarity to generate the weights of each word via  $w_j = \sigma(s_j)$ . By considering the relative importance, [Equation 17](#page-8-2) then becomes:

<span id="page-8-4"></span>
$$
\mathbf{d}^{t} = MaxPool([w_1\widetilde{\mathbf{a}^1}, w_2\widetilde{\mathbf{a}^2}, ..., w_{\gamma}\widetilde{\mathbf{a}^{\gamma}}]).
$$
\n(18)

After obtaining the textual discriminative map,  $d^t$ , the visual-textual attention consistency is achieved by making  $d^t$  to be close to the *visual* discriminative map *d v* through a Mean Squared Error (MSE) loss:

$$
\mathcal{L}_{mse} = \frac{1}{N^s} \sum_{j=1}^{N^s} ||\boldsymbol{d}_j' - \boldsymbol{d}_j^v||, \tag{19}
$$

As mentioned earlier, [subsubsection 3.2.2,](#page-6-1) we detach the encoded visual discriminative representation  $r^*$  in the decoder. The reason is that adding it as an extra visual token into the decoder will result in a size difference between the visual discriminative map and textual discriminative map ( $N^s$  vs  $N^s + 1$ ), since there are no discriminative tokens available before generating the VDM.

#### <span id="page-8-0"></span>*3.3. Objective Function*

Given the entire predicted word token sequence { $p_i$ } as the generated report and the associated ground truth report { $w_i$ }, CA-MANet is jointly optimized with the cross-entropy loss  $\mathcal{L}_{ce}$ , the binary cross entropy loss  $\mathcal{L}_{bce}$  for the multi-label classification in visual discriminative map generation and the mean square error loss L*mse* in the visual-textual attention consistency module:

$$
\mathcal{L}_{ce} = -\frac{1}{N^r} \sum_{i=1}^{N^r} w_i \cdot \log(p_i),
$$
\n(20)

<span id="page-8-3"></span>
$$
\mathcal{L} = \mathcal{L}_{ce} + \lambda \mathcal{L}_{bce} + \delta \mathcal{L}_{mse}.
$$
 (21)

Here  $\lambda$  an  $\delta$  are two hyper-parameters which balance the loss contributions.

## 4. Experiments

We validate the effectiveness of CAMANet on two commonly used RRG datasets, i.e., IU-Xray and MIMIC-CXR. Four widely used text generation evaluation metrics: BLEU{1-4} [\(Papineni et al., 2002\)](#page-16-22), Rouge-L [\(Lin, 2004\)](#page-16-23), METEOR [\(Denkowski and Lavie,](#page-16-24) [2011\)](#page-16-24) and CIDEr [\(Vedantam et al., 2015\)](#page-17-14) are employed to gauge the model performance.

<b>Dataset</b>	<b>Method</b>	<b>BL-1</b>	$BL-2$	$BL-3$	$BL-4$	$RG-L$	<b>MTOR</b>	<b>CIDR</b>
	ADAATT	0.220	0.127	0.089	0.068	0.308		0.295
	ATT2IN	0.224	0.129	0.089	0.068	0.308		0.220
	$S$ ent $SAT + KG$	0.441	0.291	0.203	0.147	0.304		0.304
	<b>HRGR</b>	0.438	0.298	0.208	0.151	0.322		0.343
<b>IU-Xray</b>	CoAT	0.455	0.288	0.205	0.154	0.369		0.277
	$CMAS - RL$	0.464	0.301	0.210	0.154	0.362		0.275
	R2Gen	0.470	0.304	0.219	0.165	0.371	0.187	
	<b>KERP</b>	0.482	0.325	0.226	0.162	0.339		0.280
	<b>CMCL</b>	0.473	0.305	0.217	0.162	0.378	0.186	
	$R2GenCMN^*$	0.475	0.309	0.222	0.170	0.375	0.191	
	<b>XPRONet</b>	0.525	0.357	0.262	0.199	0.411	0.220	0.359
	CAMANet(Ours)	0.504	0.363	0.279	0.218	0.404	0.203	0.418
	<b>RATCHET</b>	0.232				0.240	0.101	
	ST	0.299	0.184	0.121	0.084	0.263	0.124	
	ADAATT	0.299	0.185	0.124	0.088	0.266	0.118	
<b>MIMIC</b>	ATT2IN	0.325	0.203	0.136	0.096	0.276	0.134	
-CXR	TopDown	0.317	0.195	0.130	0.092	0.267	0.128	
	<b>CMCL</b>	0.344	0.217	0.140	0.097	0.281	0.133	
	R2Gen	0.353	0.218	0.145	0.103	0.277	0.142	
	R2GenCMN	0.353	0.218	0.148	0.106	0.278	0.142	
	<b>XPRONet</b>	0.344	0.215	0.146	0.105	0.279	0.138	0.154
	CAMANet(Ours)	0.374	0.230	0.155	0.112	0.279	0.145	0.161

<span id="page-9-2"></span>Table 2. Comparative results of CAMANet with previous studies. The best values are highlighted in bold and the second best are underlined. BL and RG, MTOR and CIDR are the abbreviations of BLEU, ROUGE, METEOR and CIDEr respectively.

# *4.1. Datasets*

Proposed by the Indiana University, IU-Xray <sup>[2](#page-9-0)</sup> [\(Demner-Fushman et al., 2016\)](#page-16-25) contains 7,470 X-ray images and 3,955 corre-sponding reports. The majority of patients provided both the frontal and lateral radiology images. MIMIC-CXR<sup>[3](#page-9-1)</sup> [\(Johnson et al.,](#page-16-26) [2019\)](#page-16-26) is a large chest X-ray dataset with 473,057 X-ray images and 206,563 reports provided by the Beth Israel Deaconess Medical Center. Both of these two datasets are publicly available. We follow the same data splits as [\(Chen et al., 2020\)](#page-16-4), to divide the IU-Xray dataset into train (70%), validation (10%) and test (20%) sets and remove samples without both view of images. The official data split is adopted for the MIMIC-CXR dataset.

#### *4.2. Implementation Details*

Following the same setting of previous work [\(Li et al., 2018;](#page-16-27) [Chen et al., 2020,](#page-16-4) [2021\)](#page-16-5), we utilize both images of a patient on IU-XRay by concatenating the visual tokens, and one view for MIMIC-CXR. Images are firstly resized to (256, 256) and then cropped to (224, 224) (random crop in training and center crop in inference). During the training, we randomly apply one of the operation from {*rotation*, *scaling*} to further augment the datasets. We employ the DenseNet121 [\(Huang et al., 2017\)](#page-16-21) pre-trained on ImageNet [\(Deng et al., 2009\)](#page-16-28) as our visual extractor and a randomly initialized memory driven Transformer [\(Chen et al., 2020\)](#page-16-4) as the backbone for the encoder-decoder module with 3 layers, 8 attention heads and 512 dimensions for the hidden states. The visual extractor produces  $7 \times 7$  visual tokens, thus  $N^s = 49$ .

The Adam [\(Kingma and Ba, 2015\)](#page-16-29) is used to optimize CAMANet. The learning rates are set to 1*e* − 3 and 2*e* − 3 for the visual extractor and encoder-decoder on IU-Xray, while MIMIC-CXR has a smaller learning rate with 5*<sup>e</sup>* <sup>−</sup> 5 and 1*<sup>e</sup>* <sup>−</sup> 4 respectively. λ

<span id="page-9-1"></span><span id="page-9-0"></span><sup>3</sup>https://physionet.org/content/MIMIC-cxr-jpg/2.0.0/

and  $\delta$  in Equation [20](#page-8-3) are set to 1 and 0.15 on IU-Xray, and 1 and 0.5 on MIMIC-CXR. The proportion of important words  $k$  in [Equation 18](#page-8-4) is 0.25 and 0.3 on IU-Xray and MIMIC-CXR. Note that the optimal hyper-parameters are determined by evaluating the models on the validation sets.

The same as the most promising studies reported, we adopt a beam size of 3 to balance the effectiveness and efficiency. We implement our model via the PyTorch [\(Paszke et al., 2019\)](#page-16-30) deep learning framework on Nvidia RTX6000 GPU cards.

#### *4.3. Comparisons to SOTA methods*

We compare CAMANet to 13 previous studies, i.e., *ADAATT* [\(Lu et al., 2017\)](#page-16-7), *ATT2IN* [\(Rennie et al., 2017\)](#page-17-5), *S entSAT* + *KG* [\(Zhang et al., 2020\)](#page-17-0), *HRGR* [\(Li et al., 2018\)](#page-16-27), *CoAT*[\(Jing et al., 2018\)](#page-16-0), *CMAS* − *RL* [\(Jing et al., 2019\)](#page-16-31), *R*2*Gen* [\(Chen et al.,](#page-16-4) [2020\)](#page-16-4), *KERP* [\(Li et al., 2019\)](#page-16-32), *R*2*GenCMN* [\(Chen et al., 2021\)](#page-16-5), *RATCHET* [\(Hou et al., 2021\)](#page-16-33), *T opDown* [\(Anderson et al., 2018\)](#page-16-34), *CMCL* [\(Liu et al., 2021a\)](#page-16-35), *XPRONet* [\(Wang et al., 2022\)](#page-17-15).

As [Table 2](#page-9-2) demonstrates, our proposed method achieves the best performance on all the evaluation metrics MIMIC-CXR datasets except for the RG-L metric on which CAMANet scores slightly lower (-0.2%) than *CMCL*. Nevertheless, CAMANet surpasses *CMCL* on all the remaining six evaluation metrics by a notable margin, indicating that CAMANet can generate more semantic reports rather than bias to one indicator such as precision or recall. Similar pattern can be seen on IU-Xray dataset where CAMANet obtains best scores on four out of seven evaluation metrics and is the second best performed method on the remaining three metrics.

Moreover, CAMANet outperforms the previous state-of-the-art approaches by a notable margin. For instance, CAMANet surpasses the second-best BLEU-4 and CIDEr scores by 1.9% and 5.9% respectively on the IU-Xray dataset. Similarly, a 2.1% and 0.6% improvements can be seen on BLEU-1 and BLEU-4 scores of CAMANet compared to the second-best performing method on MIMIC-CXR. Note that the MIMIC-CXR dataset is much larger and challenging and making even a small improvement proves difficult.

We mainly attribute the superiority of CAMANet to the improved cross-modal alignment achieved by the visual-textual attention consistency module, and the enriched disease-related feature representations by the proposed VDM assisted encoder. Further visualizations are provided in Section [4.7.](#page-13-0) The following ablation studies confirm the effectiveness of each component in CA-MANet.

Use of Pseudo Labels CAMANet utilizes the pseudo labels to generate the CAMs. Note that the visual extractor of CAMANET is IMAGENET pretrained. Methods *S entS AT* + *KG* [\(Zhang et al., 2020\)](#page-17-0) and *RATCHET* [\(Hou et al., 2021\)](#page-16-33) utilize pseudo labels to pre-train the visual extractor; HRGR adopts two auxiliary datasets with ground truth labels to pre-train the visual extractor; whereas KERP utilizes some manually labelled data and templates; *CMCL* [\(Liu et al., 2021a\)](#page-16-35) uses the pseudo labels to fine-tune their visual extractor and determines the visual difficulty; XPRONet [\(Wang et al., 2022\)](#page-17-15) utilizes the pseudo labels to form a cross-modal prototype-driven network. CAMANet still outperforms these methods. Moreover, the pseudo labels we used are provided with the MIMIC-CXR dataset.

# *4.4. Ablation Studies*

Here, we firstly explore the influence of each component in CAMANet including the VDM Assisted Encoder (VDMAE) and Visual-Textual Attention Consistency (VTAC) module. The following models are used to conduct the ablation studies:

• Base: The base model consists only of the visual extractor and the base encoder-decoder without other extensions.

<b>IU-Xray</b>	$BL-1$	$RI - 2$	$BL-3$	$BL-4$	$RG-L$	<b>MTOR</b>	<b>CIDR</b>	$AVG. \wedge$
Base	0.451	0.289	0.209	0.159	0.365	0.175	0.336	
$+VDMAE$	0.473	0.321	0.238	0.177	0.402	0.189	0.415	11.8%
$+VAMAE+VTAC$	0.504	0.363	0.279	0.218	0.407	0.203	0.418	$22.8\%$
<b>MIMIC-CXR</b>	$BL-1$	$RI-2$	$BL-3$	$BL-4$	$RG-L$	<b>MTOR</b>	<b>CIDR</b>	$AVG. \wedge$
Base	0.324	0.203	0.138	0.100	0.276	0.135	0.144	
$+VDMAE$	0.357	0.227	0.148	0.107	0.277	0.142	0.162	7.7%
$+VAMAE+VTAC$	0.374	0.230	0.155	0.112	0.279	0.145	0.161	$10.5\%$

<span id="page-11-0"></span>Table 3. The experimental results of ablation studies on the IU-Xray and MIMIC-CXR datasets. The best values are highlighted in bold. BL and RG, MTOR and CIDR are the abbreviations of BLEU, ROUGE, METEOR and CIDEr respectively.

<b>Input Image</b>	<b>Ground Truth:</b> Low lung volumes are present. This accentuates the	<b>Base:</b> Single portable view of the chest is compared to
PORTABLE	size of the <b>cardiac</b> silhouette which is likely mildly enlarged Mediastinal and hilar contours are likely within normal limits. A right brachiocephalic venous stent is re-demonstrated. There is crowding of the <b>bronchovascular</b> structures with probable mild <b>pulmonary</b> vascular congestion. No pleural effusion or <b>pneumothorax</b> is identified.	previous exam from. Low lung volumes are seen on the current exam. The lungs are grossly clear of confluent consolidation or large effusion. Cardiac silhouette is enlarged but stable in configuration. Osseous and soft tissue structures are unremarkable.
	<b>Base+VDMAE:</b> <b>Lung volumes</b> are low. Heart size is mildly enlarged. Mediastinal and hilar contours are unremarkable. Crowding of <b>bronchovascular</b> structures is present without overt pulmonary edema. Patchy opacities in the lung bases likely reflect areas of atelectasis. No consolidation pleural focal effusion <sub>or</sub> <b>pneumothorax</b> is present. No acute osseous abnormalities detected.	<b>Base+VDMAE+VTAC:</b> <b>Lung volumes</b> are low. This <b>accentuates</b> the size of the cardiac silhouette which appears mildly enlarged. Mediastinal and hilar contours are unremarkable. Crowding of the <b>bronchovascular</b> structures is present without overt pulmonary edema. Patchy opacities in the lung bases likely reflect areas of atelectasis. No large pleural effusion or <b>pneumothorax</b> is present. There are no acute osseous abnormalities.

<span id="page-11-1"></span>Fig. 3. An example of the reports generated by different models. Most medical terms are highlighted in different colors to better differentiate the findings of report.

- Base+VDMAE: The standard encoder in the base model is replicated with our proposed VDM assisted encoder by adding the VDM Generation and VDMAE module.
- Base+VDMAE+VTAC: This is the full CAMANet containing all our proposed components.

We present the main ablation study results in [Table 3.](#page-11-0) A remarkable improvement can be seen by adding the VDMAE module, e.g., CIDEr scores increase from 0.336 to 0.415, and 0.144 to 0.162 on IU-Xray and MIMIC-CXR benchmarks respectively. Our method gains the most significant improvements when further integrating with the visual-textual attention consistency module. In particular, the full model obtains an average of <sup>22</sup>.8% improvement over all the evaluation metrics on IU-Xray, and <sup>10</sup>.5% on MIMIC-CXR. The improvements on MIMIC-CXR are less obvious than IU-Xray since it is harder to learn a robust discriminative representation and cross-modal alignments in such a large dataset (50 times lager than IU-Xray). Section [4.7](#page-13-0) presents some qualitative results to further illustrate the model's effectiveness.

#### *4.5. Sensitivity of the Proportion of Selected Words*

To investigate the sensitivity of the hyper-parameter *<sup>k</sup>*, we vary the proportion of the selected important word tokens from 0.<sup>15</sup> to 0.35. As illustrated in [Figure 4](#page-12-0) and [Figure 5,](#page-12-1) CAMANet is not overly sensitive to this proportion. However, it is still important to strike a balance when setting the value of *k* as a small *k* may not encompass all the important words, while too large a value may introduce irrelevant words. The fluctuation on IU-Xray is relatively greater than MIMIC-CXR, which is expected since IU-Xray is significantly smaller and the reports contain larger word variance compared to MIMIC-CXR.



<span id="page-12-0"></span>Fig. 4. Effect of varying *k*, proportion of important tokens on MIMIC-CXR. (BLEU-4 score).



<span id="page-12-1"></span>Fig. 5. Effect of varying *k*, proportion of important tokens on IU-Xray. (BLEU-4 score).

# *4.6. Computational Costs*

*Training Time.* The batch size is set to 32 for IU-Xray and 64 for MIMIC-CXR. We train all the models for 30 epochs on both datasets. An early stop strategy is adopted, i.e., training stops when no improvement is seen on the validation set for more than 10 epochs. [Table 4](#page-12-2) shows the average training time of one epoch for the *Base* and *CAMANet* on IU-Xray and MIMIC-CXR. CAMANet only slightly increases the training time on MIMIC-CXR, while the increased training time is negligible on IU-Xray.



<span id="page-12-2"></span>

*The number of parameters.* Here, we compare the number of parameters of the *Base* and *CAMANet* models in [Table 5.](#page-12-3) The increase in number of learnable parameters is negligible compared to the base model.



#### <span id="page-12-3"></span>Table 5. The number of parameters of different models.



<span id="page-13-1"></span>Fig. 6. The visualizations of cross-modal attention maps for some medical terms by different models. The VDM and TDM are also shown.

#### <span id="page-13-0"></span>*4.7. Qualitative Results*

To further verify the proposed method, we provide an example in [Figure 3](#page-11-1) which shows the reports generated by different models. CAMANet appears to better capture the disease information and generate the abnormal description, e.g., *,"...This accentuates the size of the cardiac silhouette which appears mildly enlarged..."*, compared to the base model. Moreover, we visualize its generated visual discriminative map (VDM), textual discriminative map (TDM) and the cross-modal attention map from the last decoder in [Figure 6](#page-13-1) to explore whether the cross-modal alignment is truly enhanced by the proposed VTAC module. It can be seen that the *Base* model cannot learn any useful cross-modal alignments when generating the reports. Similar to the *Base* model, *Base*+*VDMAE* also fails in the cross-modal attention. This is expected since the discriminative representation is detached from the decoder. Nonetheless, owing to the enriched disease information, the *Base*+*VDMAE* model still can capture some abnormal single-model patterns, and therefore achieves improved performance compared to the *Base* model. It is clear that after adding the VTAC module, CAMANet demonstrates potent cross-modal alignment capability where the medical terms, e.g., '*lung*', focus on the associated discriminative image regions, while trivial words, e.g., '*without*', pay attention only to the background. Visualizations of the VDM and TDM further verify the effectiveness of employing a VDM as a form of pseudo label to supervise the cross-modal attention learning.

During the experiments, we found that even if a sample is wrongly classified, the model can still produce a class activation map focusing on the foreground, e.g, chest or lung, rather than the background, reducing the reliance on pseudo labels.

Finally we present further visualization results in [Figure 7.](#page-14-0) The visualizations show the reports predicted by CAMANet and the associated ground truth. We also provide the visual discriminative map (VDM), textual discriminative map (TDM), the crossattention maps of some medical terms in the inference mode and include important words in the training mode.



<span id="page-14-0"></span>Fig. 7. Some examples of generated reports by CAMANet and the associated VDM, TDM, Cross-modal attention maps and selected important words. Duplicated words in the selected important words have been removed.

#### 5. Conclusions

In this work, we propose a novel class activation map guided RRG framework, CAMANet, which explicitly leverages crossmodal alignment and disease-related representation learning. Our visual discriminative map (VDM) assisted encoder distills the discriminative information into the model via a derived discriminative representation and the self-attention mechanism. The generated VDM is then regarded as the ground truth in the proposed visual-textual attention consistency (VTAC) module to supervise the cross-modal attention learning, aimed at explicitly promoting cross-modal alignment. Experimental results on two widely used RRG benchmarks prove the superiority of CAMANet over previous studies. The ablation studies further verify the effectiveness of individual components of CAMANet. Moreover, a number of illustrative visualizations and discussions are provided to inspire future research in this area.

## Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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## Source code

We will be providing public access to Python code and relevant model data in due course.

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